Determination of Bumper Styling and Engineering Parameters to Reduce Pedestrian Leg Injuries

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ABSTRACT
The European Commission is proposing legislation aimed at reducing the severity of injuries sustained by pedestrians in the event of an impact with the front-end of a motor vehicle. One aspect of this proposed legislation is reducing the pedestrian's leg injuries due to contact with the bumper and frontal surfaces of a vehicle, assessed using a 'pedestrian leg impact device,' or 'leg-form.'

This proposed legislation presents the challenge of designing a bumper system which achieves the required performance in the leg-form impact—without sacrificing the bumper's primary function of vehicle protection during low-speed impacts. The first step in meeting this challenge is to understand what effects the front-end geometry and stiffness have on the leg-form impact test results. These results will then need to be compared to low-speed impact performance to assess if the two requirements are compatible.

This paper describes an investigation—using concept Finite Element models and a front-end variable geometry vehicle test buck—of the styling and engineering trade-offs for a pedestrian safe bumper system.

INTRODUCTION
Over the past three decades, car manufacturers and legislators have worked diligently to enhance the safety of vehicle occupants. As a direct result of this effort, the number and severity of automotive accidents resulting in injury to the occupants is on the decline.

One area of automotive safety that has received less attention, however, is the protection of pedestrians. While research into pedestrian accidents began in the late 1970's, it was not until recently that considerable effort has been focused on developing a vehicle performance requirement. In 1990, the EC\(^a\) commissioned a group of European automotive safety agencies (TRL\(^b\), INRETS\(^c\), BASI\(^d\), and TNO\(^e\) – the EEVC\(^f\) Working Group 10) to develop a pedestrian impact test procedure that was both repeatable and accurate; replicating a typical pedestrian impact event. The group's original proposals were published in 1991 [1]. These consisted of three sub-system impact test procedures targeted at further reducing the severity of leg, thigh / pelvis, and head injuries (the three most commonly injured areas in a pedestrian impact) at velocities up to 40 km/h (25 mph). The test procedures were proposed as a draft EC Directive in February, 1996 [2]. In addition, these test procedures are being used to evaluate vehicles in the new Euro-NCAP\(^g\) test program sponsored by the U.K. DoT\(^h\), FiA\(^i\), SNRA\(^j\), et al.

The three impact modes presented in the EEVC proposals are (Figure 1):

1. Leg impacts to the vehicle's bumper system and frontal surfaces using a 'free-flight' pedestrian leg impactor (a 'leg-form') [3].
2. Thigh impacts to the vehicle's hood/bonnet leading edge with a guided thigh impact device [4].
3. Adult and child head impacts to the vehicle's hood-top with two free-flight head impact 'head-forms' [5].

This paper reviews some of the results of an investigation of the styling and engineering implications of the proposed leg impact requirements. In this test procedure, a leg

\(^a\) EC: European Commission (provides overall policy direction to each of its 12 member states).
impactor (a detailed discussion of this device is included in the "Leg-Form Impactor" section of this paper) is propelled at a stationary vehicle at a velocity of 40 km/h (approximately 25 mph). The velocity is parallel to the longitudinal axis of the vehicle and can be performed at any point across the front face between the vehicle corners. For this impact event, the proposed performance requirements are:

- Tibia Acceleration (near knee) < 150 g
- Lateral Knee Bend Angle < 15 degrees
- Lateral Knee Shear Deformation < 6 mm

BACKGROUND

The bumper system has the largest influence on the vehicle's leg impact performance, with the hood leading edge playing a secondary role in limitation of knee bending. Many of the previous papers on this subject are very generic in nature, stating which bumper parameters influence the leg impact performance. In addition, most of the prior work has not used one of the current leg-form impactors.

This earlier work, however, has been essential in the development and implementation of the current test series. In particular, much of the prior work [6-16] has made general recommendations for bumper design which were included in the basic designs tested:

- Lower bumper height-to-ground has been projected to reduce lateral knee bend angle [6,7,8,9,10,11,12], while potentially increasing head impact speed [13].

- A structural lower stiffener [13,14,15] has been proposed as an alternative to a lower bumper height.
- A compliant (soft) bumper system [16] has been used to reduce tibia acceleration, but may reduce vehicle low-speed damage protection.

In order to minimize the influence on (a) the vehicle's styling and (b) the ECE-42 [17] (low-speed damageability) performance, bumper heights should be maintained. Because of this, a structural lower stiffener was added below the existing bumper to reduce lateral knee bend angles. Bumper height-to-ground variation was limited to +/- 25 mm.

Although a very compliant (hollow) bumper system has been shown [16] to perform well in the pedestrian leg impact, this would result in poor performance in the ECE-42 test. Because of this, the following adaptation of a typical bumper system design was chosen as the preferred solution:

- Rigid bumper beam or lower cross-member
- Locally compliant energy-absorbing foam
- Flexible plastic fascia
- Structural lower stiffener

In addition to selection of the bumper system configuration, information on the specific shape and stiffness of these components is also required. The focus of this study was to develop a better understanding of which shape and stiffness characteristics are beneficial to leg-form impact performance.
The shape (geometry) and stiffness of a vehicle's front-end are the most significant contributors to pedestrian leg-form impact performance. In order to investigate the specific effects of each characteristic, an adjustable parameterized vehicle front-end design was needed. In particular, the ability to change the bumper (foam) and lower stiffener dimensions, locations, and stiffnesses was required.

To this end, a 'Variable Front-End Buck' which represents the front-end design of a typical European passenger car was developed. It included a bumper, grille, hood/bonnet, and lower stiffener (added below the bumper beam and foam). The buck allowed front-end shape (geometry) and engineering (stiffness) design characteristics to be changed between tests. It represented a 600 mm section across a vehicle front-end (ignoring any curvature). A diagram of the buck (Figure 2) identifies the adjustable geometry and stiffness factors. Table 1 provides a definition of each of the factors.

The design of the Buck was significantly influenced by the CAE \(^{(a)}\) Concept Model development and the results of the CAE DOE \(^{(b)}\) (see CAE APPROACH, below). The CAE Concept Model development process identified how and where to attach components. It also indicated that the lower stiffener should have a 'diamond-shaped' cross-section to provide for uniform collapse during the impact. The CAE model also showed that the flexible fascia over the bumper foam influenced the way the foam absorbed energy.

The CAE DOE provided an initial indication of which factors were most important to pedestrian leg-form impact performance. These factors were then included in the Buck testing. In addition, the CAE DOE showed that the lower stiffener sizes initially selected (see Table 3) were too far apart (this factor overwhelmed the others in the DOE). Because of this, different sizes were chosen during the Variable Front-End Buck testing (see Table 5).

**LEG-FORM IMPACTOR**

Pedestrian leg impact performance is assessed through the use of a 'leg-form' impactor. The impactor is constructed from two steel tubular structures (the 'femur' and 'tibia') with prescribed masses, centers of gravity, and moments of inertia. These structures are joined by a knee joint allowing two degrees-of-freedom—'lateral knee bending' and 'lateral knee shear,' hereafter referred to as simply 'bend' and 'shear.' The entire impactor is wrapped

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\( ^{(a)}\) CAE - Computer-Aided Engineering, including Finite Element Analysis (FEA).

\( ^{(b)}\) DOE - Design of Experiments: A formal process for designing an experiment to get the most information from the least amount of tests. The experimental designs used in this work are more closely associated with Taguchi DOE method than Classical DOE.
in 25 mm of Confor™ 'flesh' foam and 6 mm of Neoprene 'skin'.

The characteristics of the knee in shear and bend are specified in terms of quasi-static force-displacement corridors, shown in Figure 3. Note that these tolerance bands are quite wide, especially for quasi-static shear tests. This is particularly true for bend, where the non-linear relationship between bending load and angle (the metric) exaggerates variability in the measured response. The full certification procedures can be found in the draft regulatory document [2].

Initial prototype leg-form ligament designs, as proposed by INRETS [3], attempted to satisfy both requirements by using a pair of metal non-linear 'ligaments' able to deform in both bend and shear modes. It was soon noted that this design suffered instability of the ligament when subjected to bend, and metric cross-talk between bend and shear. As a consequence of this, TRL proposed an alternative design in 1995 for the leg-form which separated the bend and shear mechanisms, allowing each to act independently. This solved the instability issues associated with the INRETS design and simultaneously reduced cross-talk [18]. The bend characteristics continued to be simulated through the use of non-linear ligaments, with the shear compliance achieved through the use of a linear shear spring.

The TRL design has a new concern not seen in the INRETS design—because the shearing displacement is controlled by an elastic spring, the femur and tibia segments can oscillate relative to each other. This 'shear resonance' not only affects the measurement of shear in the knee, but also the acceleration at the top of the tibia segment. TRL is in the process of revising the design to eliminate this concern.

Because of this uncertainty, neither design was used in this investigation. Instead, a MIRA(b)-developed hybrid design, internally known as the 'Simplified Leg-Form,' was used. This has approximately the same mass distribution and bending characteristics as is specified in the EEVC test procedure [1]. However, a shearing mechanism is not included in the design due to the concerns outlined above. It is the opinion of the authors that any system which meets the bend and acceleration requirements would require few changes to also meet the shear requirement.

Comparisons between the mass properties and bending characteristics of the Simplified Leg-Form and the EEVC proposal are shown in Table 2 and Figure 4. While these differences may change the magnitudes of the individual test results, it is the authors' opinion that the trends in the responses will be consistent. Because of this, the bend and acceleration results will only be reported relative to the overall average of the test results.

**Table 2: Leg-Form Mass Properties**

<table>
<thead>
<tr>
<th></th>
<th>EEVC Proposal</th>
<th>Simplified Leg-form</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>FEMUR</td>
<td>TIBIA</td>
</tr>
<tr>
<td>mass (kg)</td>
<td>8.6</td>
<td>4.8</td>
</tr>
<tr>
<td>I (kg-m²)</td>
<td>0.127</td>
<td>0.120</td>
</tr>
<tr>
<td>CG (mm)</td>
<td>217</td>
<td>233</td>
</tr>
</tbody>
</table>

**CAE APPROACH**

To help shorten product development cycles, a CAE model for the leg impactor and a vehicle modeling methodology have been developed. In addition, these tools were used to determine the initial design for the Variable Front End Buck. All analyses presented in this...
paper have been performed with RADIOSS® version 3.1H or later on a Cray C90.

DESCRIPTION OF MODEL

The simplified impacter was modeled with only nine basic parts (Figure 5). They were:

- Femur and Tibia Skins (rubber)
- Femur and Tibia Flesh (foam)
- Femur and Tibia Cores
- Femur and Tibia Rigid Bodies
- Knee Spring

Since this model does not include shear at the knee, a very simple knee model definition was applied. First, the femur and tibia segments were modeled full-length (eliminating the gap between the tibia and femur segments). Knee rotation was then allowed by specifying no interfaces between these two segments in the model. The segments were joined at the center by a zero-length general spring element.

All degrees-of-freedom for the spring element were constrained with the exception of lateral bending. For this degree-of-freedom, a non-linear function was used to define the bending properties of the knee. Anisotropic hardening was used to represent the behavior of the physical knee ligaments, based on the leg impacter static bending certification corridor.

Figure 6 shows the finite element representation of the variable geometry buck. It includes a foam block supported rigidly at its rear face, a bumper fascia to correctly simulate the distribution of force and energy into the foam, and a lower stiffener. In addition, a grill and hood leading edge are included to correctly support the upper portion of the leg during the later stages of the impact.

The Grille, Fascia and Stiffener are all modeled using material Type 2 (elastic-plastic). The foam is modeled using material Type 33 (low density viscoelastic-plastic foam) based on material properties, supplied by Bayer AG, from dynamic crush tests at 4 km/h. The viscous nature of polyurethane (PU) foams however, means that the properties are often significantly different at higher impact velocities such as the 40 km/hr used in pedestrian leg impact tests. For this reason the supplied data was arbitrary scaled, based on previous high speed PU foam testing experience.
CAE BUCK RESULTS

A typical sequence of events is illustrated in Figure 7. Maximum tibia acceleration typically occurs between 5 and 10 milliseconds after initial contact with the bumper system. Maximum bending angle typically occurs 10 to 15 milliseconds later.

For the DOE analysis to produce valid engineering guidelines, the average of the test results should be near the required target values (from the proposed legislation). The acceleration results of this CAE DOE were well distributed around the 150 G target. However, the knee bend angles were centered around 20 degrees, five degrees higher than the target of 15 degrees. Because of this, the stiffener locations for the subsequent variable buck testing were changed to ensure well-balanced results.

The DOE analysis was performed as an ANOVA (Analysis of Variance) using Minitab. A significance criteria of 90% (1.0 - P > 0.9) was used to evaluate the factors and interactions. This analysis indicated that all four factors were significant relative to the knee bend angle results. However, only two of the factors, K-Bump and K-Stiff, were significant for the acceleration results. In addition, none of the first-order interactions were found to be significant for either of the measured results.

The DOE analysis also consisted of viewing main effects plots to check for curvature in the responses and determine whether the ranges selected for the CAE model were appropriate to be used in the physical testing. From the main effects plots, it was observed that the stiffener stiffness (K-Stiff) was linear in both response variables. Also, K-Stiff was found to have opposite effects on the two measured results: Higher spoiler stiffness resulted in lower bend angle, but higher acceleration. Because of this, the K-Stiff factor levels were changed for the physical testing, based on further CAE optimization of this parameter.

<table>
<thead>
<tr>
<th>Table 3: Parameter Levels in CAE DOE</th>
</tr>
</thead>
<tbody>
<tr>
<td>Factor</td>
</tr>
<tr>
<td>----------</td>
</tr>
<tr>
<td>X-grille</td>
</tr>
<tr>
<td>H-bump</td>
</tr>
<tr>
<td>K-BUMP</td>
</tr>
<tr>
<td>X-BUMP</td>
</tr>
<tr>
<td>Z-bump</td>
</tr>
<tr>
<td>K-STIFF</td>
</tr>
<tr>
<td>X-STIFF</td>
</tr>
<tr>
<td>Z-stiff</td>
</tr>
</tbody>
</table>

ANALYTICAL PROCEDURE

In order to minimize the number of CAE runs required and to maximize the lessons learned from them, a DOE approach was chosen. Of the eight parameters listed in Table 1, the four deemed to be most significant from previous experience were selected as 'factors' in the DOE. Each of these factors was allowed to take one of three possible values, as shown in Table 3 (Z-stiff was chosen to be dependent on X-stiff in order to maintain a constant approach angle). All other parameters were fixed at levels typically observed on small European cars. For reference, the pedestrian leg-form knee height is defined to be 494 mm from the ground.

The orthogonal array chosen for the DOE was the M27 'probing' matrix. This allows all four of the three-level factors to be used while leaving the main effects and first-order interactions 'clear' (i.e., not confounded with each other).
VARIABLE BUCK TESTING

The test setup, the experimental design, and the DOE results for the physical test series using the Variable Front-End Buck are presented in this section.

TEST RIG CONFIGURATION

The test setup consisted of the Variable Front-End Buck rigidly mounted to a steel bed-plate placed in front of a Bendix Impactor. There was a carriage attached to the impactor to support the pedestrian leg-form during the initial acceleration of the cylinder. The carriage was stopped after the initial acceleration was complete, allowing the leg to travel the last 0.6 m to the Variable Front-End Buck in free flight at 40 km/h.

A schematic of the Buck was shown in Figure 2. A post-test photograph of the Buck is shown in Figure 8. Sliding attachments and spacer blocks were used for the bumper and stiffener vertical and longitudinal positioning. The plastic grille assembly was attached only at the outboard edges of the Buck, allowing it to bend during the impact. The hood inner panel was attached at the centerline of the buck to simulate a hood latch. The bumper and stiffener components were replaced after each impact. The hood and grille were inspected after each impact and replaced if any structural damage was found.

DESIGN OF EXPERIMENT (DOE) APPROACH

In order to minimize the number of experimental runs, a Screening DOE approach was used. The key questions to be answered by the DOE were:

- Which factors are most critical to the pedestrian leg-form impactor performance?
- Which factors have a non-linear relationship to the responses?
- What are the best settings for the critical factors?

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*Bendix Impactor - a hydraulic open loop actuator used as a guided mass accelerator to push 9 to 340 kg from 8 to 80 km/h.*
The second question led us to adopt an M18 experimental design, allowing more than two levels for each factor. This design, shown in Table 4, spreads interaction terms across many columns to minimize their influence on a single main effect. Therefore main factor interactions cannot be studied directly with this matrix. This was not a concern for this DOE, since these interactions were found to be weak in magnitude during the CAE Buck analysis.

A total of six factors were changed during the testing. This left two columns of the matrix empty to establish the level of noise in the system. Also, one repeat run was performed, to establish the repeatability of the experiment. The six factors and their settings are listed in Table 5. These settings were chosen based on the CAE DOE results. In particular, note that X-Stiff has been extended to move the stiffener in front of the bumper leading edge (+30). Also, K-Stiff was reduced to two levels since its response was found to be linear in the CAE DOE. These two levels were chosen in an attempt to achieve Knee Bend Angle results centered around the target of 15 degrees. While reading this table, recall that the leg form knee height is 494 mm from ground.

ANALYSIS OF RESULTS

The experimental results were analyzed using the Matrix. Table 4: M18 DOE Matrix

<table>
<thead>
<tr>
<th>RUN</th>
<th>COLUMN</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>-1</td>
</tr>
<tr>
<td>2</td>
<td>-1</td>
</tr>
<tr>
<td>3</td>
<td>-1</td>
</tr>
<tr>
<td>4</td>
<td>-1</td>
</tr>
<tr>
<td>5</td>
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<td>-1</td>
</tr>
<tr>
<td>9</td>
<td>-1</td>
</tr>
<tr>
<td>10</td>
<td>0</td>
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<tr>
<td>11</td>
<td>0</td>
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<tr>
<td>12</td>
<td>0</td>
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<tr>
<td>17</td>
<td>0</td>
</tr>
<tr>
<td>18</td>
<td>0</td>
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</tbody>
</table>

Table 5: Parameter Levels for Test DOE

<table>
<thead>
<tr>
<th>Factor</th>
<th>Levels</th>
<th>Unit</th>
</tr>
</thead>
<tbody>
<tr>
<td>X-grille</td>
<td>-</td>
<td>+1</td>
</tr>
<tr>
<td>H-bump</td>
<td>65</td>
<td>-</td>
</tr>
<tr>
<td>K-BUMP</td>
<td>125</td>
<td>155</td>
</tr>
<tr>
<td>X-BUMP</td>
<td>110</td>
<td>150</td>
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<tr>
<td>Z-BUMP</td>
<td>420</td>
<td>445</td>
</tr>
<tr>
<td>K-STIFF</td>
<td>1.75</td>
<td>4.00</td>
</tr>
<tr>
<td>X-STIFF</td>
<td>-30</td>
<td>+30</td>
</tr>
<tr>
<td>Z-STIFF</td>
<td>240</td>
<td>270</td>
</tr>
</tbody>
</table>

Response Surface Model (RSM) method in Minitab version 9.2. Two types of analysis were performed:

- Statistical significance was determined by calculating the coefficient of determination (R²) for each factor. Significance was defined to be greater than 90%.
- Box-plots were produced to illustrate the effect of each factor on the results.

Applicability of the results is limited to the ranges of values which were tested. Some extrapolation is probably acceptable, but caution should be exercised.

Five factors were found to be significant for the maximum Knee Bend Angle. These factors and their statistical significance are listed in Table 6. This table also includes an assessment of whether the response from that factor is essentially linear or non-linear. Figure 9 contains box-plots of the results for each significant factor. To focus on the trends rather than the absolute values, the overall Knee Bend average was subtracted out before plotting.

Table 6: Significant Factors for Knee Bend Angle

<table>
<thead>
<tr>
<th>FACTOR</th>
<th>SIGNIFICANCE</th>
<th>LINEAR?</th>
</tr>
</thead>
<tbody>
<tr>
<td>K-Stiff</td>
<td>0.99</td>
<td>YES(\textsuperscript{b})</td>
</tr>
<tr>
<td>X-Stiff</td>
<td>0.99</td>
<td>YES</td>
</tr>
<tr>
<td>Z-Bump</td>
<td>0.99</td>
<td>YES</td>
</tr>
<tr>
<td>X-Bump</td>
<td>0.94</td>
<td>YES</td>
</tr>
<tr>
<td>Z-Stiff</td>
<td>0.93</td>
<td>NO</td>
</tr>
</tbody>
</table>

\textsuperscript{a} Box-plot: A plot showing the mean and +/- one standard deviation for each level of a given factor. The mean is shown as a horizontal line and a "box" extends above and below to the standard deviations. 
\textsuperscript{b} K-Stiff was only tested at two levels. It is assumed to be linear based on the CAE results discussed earlier.
Two factors were found to be significant for the maximum Tibia Acceleration. These factors are listed in Table 7. Figure 10 contains box-plots of the results for these factors. The overall Tibia Acceleration average was subtracted out before plotting.

**CAE CORRELATION**

A study is currently underway to correlate the CAE Concept Model results to the Variable Front-End Buck test results. Preliminary results from this study have indicated the difference in mass properties (especially tibia C.G.) noted in Table 2 has a significant effect on the knee bend angle results in the CAE Concept Model. In addition, the correlation study has identified a significant concern with the specification of the knee ligament bending corridor. In an attempt to achieve correlation between the CAE and test results, the knee ligament bending curve used in the CAE model was varied to correspond to (a) the top of the corridor, (b) the bottom of the corridor, and (c) the actual curve generated from the ligaments used in the testing. These changes resulted in knee bend angles which were 10 degrees apart, from 9 to 19 degrees for a single configuration. This variation

<table>
<thead>
<tr>
<th>FACTOR</th>
<th>SIGNIFICANCE</th>
<th>LINEAR?</th>
</tr>
</thead>
<tbody>
<tr>
<td>X-Stiff</td>
<td>0.98</td>
<td>YES</td>
</tr>
<tr>
<td>X-Bump</td>
<td>0.92</td>
<td>NO</td>
</tr>
</tbody>
</table>

Table 7: Significant Factors for Tibia Acceleration
indicates that the exact bending curve of the knee ligaments used in a test will significantly affect the bend angle results, even if the ligaments fall within the specification.

**DISCUSSION**

Table 6 and Table 7 indicate that the location and stiffness of the lower stiffener are the most significant of the investigated factors. In addition, the bumper foam height and depth play an important, though lesser, role. These results are in agreement with the recommendations and suggested foam stiffness previously reported, with the exception of the bumper foam stiffness, which was not found to be significant within the ranges tested in this study. The current work adds quantified results to the previous recommendations—identifying the relative importance of each factor and its effects.

At this point it is important to re-iterate that the results presented are only valid in the ranges tested. In particular, the experimental results suggest that bumper foam stiffness is not a significant parameter in pedestrian leg impact. This observation is only applicable within the stiffness ranges tested (Table 5) – from 0.5 to 1.0 times the stiffness of a typical European bumper energy absorber. The authors believe that the ranges tested for this parameter were too close to identify its critical nature which will likely appear when the stiffness is increased or decreased outside of this range.

As far as the authors are aware, the lower stiffener is a new component not used on current vehicles. Because of this, any issues associated with its addition to the vehicle need to be identified. Several concerns become apparent when considering the addition of this stiff component projecting ahead and below the bumper:

- The stiffener may increase the likelihood of injury to the tibia, fibula, or ankle joint. This possibility has not yet been investigated since the proposed legislation offers no method for measuring ankle or lower tibia injury (the acceleration is measured near the top of the tibia segment on the leg-form).
- The stiffener may increase the velocity of the thigh/pelvis and head impacts by increasing the speed of the pedestrian's rotation around the vehicle's leading edge.
- High-speed impact performance may be affected, depending on the attachment points and stiffness of the stiffener.
- Low-speed damageability performance will be affected since the stiffener will likely contact some obstacles before the bumper.
- The overall vehicle length will most likely increase, potentially forcing changes to manufacturing plants or shipping operations.

This study focused on centerline impacts in controlled conditions. Designing a stiffener with the same stiffness characteristics across the entire width of a vehicle remains an open issue.

Three issues associated with the bumper foam depth and position are:

- Deeper bumper foams may affect high-speed impact performance by changing the initial vehicle deceleration seen by the airbag sensor.
- Lower bumper heights may affect ECE-42 performance by moving the bumper system below the specified impact height.
- Deeper bumper foams will result in an increase in the vehicle length, potentially forcing changes to manufacturing plants or shipping operations.

In addition, any of the identified changes to the bumper system will certainly result in increased cost and weight to the vehicle designed to meet the proposed pedestrian leg-form impact requirements.

**CONCLUSIONS**

There are several styling, packaging, and stiffness factors in the design of a vehicle's front-end which influence pedestrian leg-form impact performance. The focus of this work was to determine which of several selected factors significantly affect the impact test results.

The paper reviewed the development of a standard proposing requirements for pedestrian leg impact. Previously published bumper design recommendations for pedestrian impact were presented, followed by a discussion of issues associated with the two current proposed leg-form impactors.

The methodology utilized a CAE leg impactor model and front-end concept model in addition to a Variable Front-End Buck to investigate the effects of various front-end design parameters on pedestrian leg-form impacts. Six front-end factors were investigated in a DOE using the buck and CAE concept model. The trends identified from the experimental results were found to be consistent with CAE results. In addition, during the CAE correlation, the wide knee ligament certification corridor was found to result in a potentially non-robust measurement of lateral knee bend angle.

The key bumper design factors associated with pedestrian leg-form impact performance were identified. Issues associated with introducing the vehicle front-end design changes suggested by the experimental results were identified for future study.
ACKNOWLEDGEMENTS

The authors gratefully acknowledge the assistance of the following individuals in this work:

- Glenn Klecker, who had the initial idea of a Variable Front End Buck.
- Karin Rothacker, who helped develop the 'Simplified Leg-form' and coordinated the Buck testing.
- Klaus-W. Huland of Bayer AG, who provided the foam samples used in the testing.

REFERENCES