# THE INFLUENCE OF MYOBLAST IMPLANTATION ON ARTERIOGENESIS IN MICE WITH DIET-INDUCED OBESITY

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by

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# PROJECT INFORMATION



## ABSTRACT

The Influence of Myoblast Implantation on Arteriogenesis in Mice with Diet-Induced Obesity

#### Rayana E. Gutierrez

Peripheral arterial occlusive disease (PAOD) is characterized by atherosclerosis, which is the buildup of plaque, consisting largely of cholesterol, in the arterial walls. This plaque accumulation eventually blocks blood flow to the limbs, causing symptoms such as intermittent claudication and tissue death in cases of critical limb ischemia. The body compensates for the reduced perfusion by enlarging pre-existing bypass arteries, known as collaterals, in a process called arteriogenesis. However, in many cases, collateral networks constructed through arteriogenesis fail to enlarge sufficiently or function effectively in patients. Therefore, the development of a therapeutic intervention specifically targeting this process would offer a valuable solution for improving blood flow and facilitating tissue perfusion. Obesity and its comorbidities induce PAOD by promoting atherosclerosis, endothelial dysfunction, and impaired vascular function, so it is critical to analyze the degree of collateral remodeling following arteriogenesis in obese subjects to understand if the phenotype impacts the effectiveness of regenerative treatment. This study aims to determine whether myoblast implantation enhances collateral growth after induced ischemia in the hindlimbs of mice with diet-induced obesity (DIO) and in lean mice. PAOD was mimicked in all subjects by occluding blood flow in the femoral artery with a suture-based ligation. A thermally responsive, injectable polymer containing myoblasts, or no cells, was injected under the gracilis anterior, just deep to the targeted collateral. After 7 days post-operation, the polymer was removed and prepared for assessment. To assess the degree of collateral remodeling, perfusion fixation and vascular casting were performed, with subsequent removal of the anterior gracilis muscle for imaging and measuring vessel luminal/abluminal diameters and calculating arterial wall thickness. The analysis of the study revealed that there was no notable difference in collateral remodeling in the subjects that received the cell treatment and no difference in collateral diameters between the phenotypes (DIO and lean). However, the arterial wall thickness was larger in mice with DIO, regardless of the treatment received. Overall, the outcome of the experiment suggests that arteriogenesis was not enhanced by myoblast implantation in obese subjects.

Keywords: arteriogenesis, atherosclerosis, cell transplantation, collateral arteries, myoblasts

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"Enthusiasm is common. Endurance is rare."

-Angela Duckworth

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## <span id="page-7-0"></span>**INTRODUCTION**

Peripheral Arterial Occlusive Disease (PAOD) is a cardiovascular illness that affects over 200 million people worldwide, with 6.5 million being patients over the age of 40 in the United States [1, 2]. PAOD occurs due to atherosclerotic plaque build-up inside of the arteries, typically in the abdominal aorta, iliac, and femoral arteries. Risk factors include diabetes, dyslipidemia, hypertension, and smoking [1, 3]. Even

in approximately half of the cases where individuals are asymptomatic, the presence of PAOD indicates systemic atherosclerosis and an elevated risk of heart disease and stroke [4]. In the early stages of atherosclerosis, the blood vessels adapt by dilating to optimize blood flow through the plaque-filled vessel [1]. However, once the vessels reach their dilation limit, the plaque continues to obstruct the arterial lumen, as seen in **Figure 1**, leading to reduced blood flow to the distal extremities and causing symptoms such as muscle pain, cramps, and fatigue [1,5]. If left untreated without revascularization, the risk of



**Figure 1. Blood flow in a healthy artery and in an atherosclerotic artery.** PAOD entails the accumulation of plaque in the arteries, leading to inadequate blood flow and oxygen levels in the distal extremities [5].

amputation within 6 months is 19%, which increases to 23% within 1 year [5]. Critical ischemic conditions resulting from PAOD lead to approximately 150,000 amputations in the United States [6]. Unfortunately, 20% of these amputations result in death within five years due to poor healing conditions [7].

The treatment options for patients with PAOD depend on the severity of their condition and associated symptoms. Exercise therapy is recommended for ambulatory patients to improve blood flow and slow disease progression [1]. Antiplatelet medications like acetylsalicylic acid (ASA), pentoxifylline, and cilostazol are prescribed to prevent blood clot formation, but their efficacy varies, and they may cause

adverse effects such as gastrointestinal bleeding and anemia. These drugs can also not be taken by patients with a history of congestive heart failure [1, 8]. In cases where physical or pharmaceutical therapies are ineffective, endovascular procedures like balloon angioplasties or stent placements are considered [7]. However, arterial restenosis, or narrowing of the vessels caused by smooth muscle cell proliferation in response to vessel damage, is a common complication after these interventions. Approximately 200,000 stents are placed in the femoral and popliteal arteries of PAOD patients each year?, and 30-40% of these cases experience in-stent restenosis within 2-3 years [9]. Furthermore, restenosis occurs in 60% of cases within 12 months following balloon angioplasty [7].

A potential solution to prevent amputation and reduce the need for surgical interventions lies in the enlargement of natural bypass arteries, emphasizing the importance of understanding the underlying

mechanisms by which the body naturally facilitates this process. In response to an arterial occlusion, natural bypass collaterals undergo arteriogenesis, involving outward vascular remodeling in these vessels (**Figure 2**). More specifically, the obstruction caused by plaque buildup results in an elevated pressure gradient and shear stress between the proximal and distal arteries, leading to the enlargement of collateral vessels as they optimize blood flow



**Figure 2. Collateral Vessels.** Collaterals are natural bypass vessels that redirect blood around a blockage or obstruction in an artery, reinstating and normalizing the flow of blood to the surrounding and distal tissue [10].

to normalize shear forces [11]. At a cellular level, the endothelial cells lining the vessel lumen respond to increased shear stress by transducing the mechanical stimuli into intracellular activation of chemokines and adhesion molecules, which in induce the recruitment of monocytes [12].

These recruited monocytes differentiate into macrophages, which further enhance the inflammatory environment by secreting growth factors suchs as basic fibroblast growth factor (bFGF) and tumor necrosis factor-alpha (TNF-α). Moreover, macrophages produce matrix metalloproteinases, enzymes that degrade the elastic lamina and extracellular matrix (ECM) of the vessel. The combined effects of bFGF and TNF-α promote the proliferation of vascular smooth muscle cells (VSMCs), leading to the rearrangement and expansion of ECM components such as collagen and elastin. This remodeling process contributes to the enlargement of the internal elastic lamina and tunica media layers, resulting in a larger vessel size and enhanced perfusion to the distal tissues (**Figure 3**) [12] .



**Figure 3. Macrophage-mediated Arteriogenesis.** In unobstructed vasculature, blood flow is directed through the conductance artery (left). When the conductance artery is occluded, the increased shear stress is detected by the endothelium in the pre-existing collaterals, signaling for monocyte recruitment (middle). Monocytes differentiate into macrophages that induce cellular processes for arteriogenesis, ultimately restoring adequate perfusion (right) [13].

Although various regenerative solutions, including gene, protein, and cell-based therapies, have been tested in clinical trials for their efficacy in treating PAOD, only a few trials have successfully demonstrated increased arteriogenesis in humans compared to preclinical animal trials [14]. Examples of therapeutic products studied include bFGF protein, VEGF gene-plasmid, bone marrow-derived mononuclear cells (BMMNCs), peripheral blood-derived cells, and mesenchymal stem cells [14, 15]. The outcomes of these therapeutic treatments in human trials have been criticized for their uncontrolled nature and small sample sizes, whereas larger randomized clinical trials have failed to replicate the positive results achieved in smaller studies [14]. Conversely, animal studies consistently demonstrate successful enhancement of arteriogenesis, including murine and rabbit hindlimb models with induced arterial occlusion and monocyte implantation [16, 17]. The reasons for the disparities between human and animal trial outcomes remain uncertain, but it is likely that challenges in managing physiological variability contribute to these differences [14].

It is important to recognize that obesity, frequently observed in patients with PAOD, is due to excessive fat accumulation and triggers oxidative stress, insulin resistance, inflammation, and ultimately, endothelial dysfunction [18]. Since obesity has a significant impact on arterial remodeling, it becomes crucial to replicate these physiological characteristics in animal models during preclinical studies. There is a correlation between obesity and lower circulating levels of endothelial progenitor cells (EPCs), which are cells that contribute to vascular repair and regeneration through direct and paracrine mechanisms [19]. The diminished presence of EPCs in the blood may lower the efficiency of arteriogenesis and reduce endothelial function in collaterals in the cases of PAOD in obese patients. Due to the scarcity of clinical trials substantiating the efficacy of EPC injection and other cell-based therapies (such as bFGF protein, BMMNCs, and mesenchymal stem cells) in the treatment PAOD, it is crucial to explore alternative promising treatments such as myoblast implantation.

Myoblasts, a type of progenitor cell found in skeletal muscle that is responsible for the regeneration of muscle fibers, have been thoroughly observed in the applications of stem cell therapy, gene therapy, and tissue engineering [20]. Upon activation in response to muscle fiber injury, satellite cells undergo proliferation and differentiation into myoblasts, and eventual maturation into myocytes and myotubes to generate new muscle fibers, thereby aiding in the repair and regeneration of damaged muscle tissue [21]. As previously mentioned, macrophages play a vital role in regulating arteriogenesis, and although the connection is not fully understood, researchers have noted that activated myoblasts may be positively influenced by the presence of macrophages [22]. The possible interaction between skeletal muscle

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progenitor cells and macrophages amplifies the significance of investigating myoblasts as essential components for enhancing arteriogenesis. A previous study has shown that implanted myoblasts seeded onto gelatin constructs into mice with diet-induced obesity (DIO), following femoral artery ligation, improved arteriogenesis and enhanced functional vasodilation [23]. Building upon this research, the study discussed in this paper aimed to replicate the previous work, by use of a clinically applicable cell delivery construct which consists of a thermally responsive, injectable polymer that remains in liquid form inside a syringe until exposed to the body temperature of approximately 37°C. Injecting the cell vehicle may prove to be safer and more efficient to use in future clinical cases relative to the gelatin construct utilized in the previous study. The hypothesis of this experiment is that myoblasts injected under the gracilis muscles following femoral artery ligation, will enhance arteriogenesis within the collaterals in mice with DIO, assessed at 7 days after the operation.

#### <span id="page-11-0"></span>METHODS

#### <span id="page-11-1"></span>*Animals*

Every animal procedure involved in this study was approved by the Institutional Animal Care and Use Committee (IACUC) of California Polytechnic State University. The subjects consisted of 17–20-weekold C57BL/6 male mice (n=22) that were received from The Jackson Laboratory. Upon delivery to the university vivarium, the mice were housed in groups of 4-6, in cages with ad libitum access to food and water. The vivarium room was consistently regulated for temperature and lighting conditions, following a 12-hour light and dark cycle. The conditions of the mice, feed, water, and room were inspected daily. Following their arrival at the facility, the mice continued their specialized diet of either control feed (10% fat) for lean mice (n=5), or treatment feed (60% fat) for mice with DIO (n=17). The subjects were acclimated to the housing environments approximately two weeks prior to the first surgery. Following a survival procedure, the mice were reintroduced to the vivarium and placed in pairs, each with their designated food, until the 7-day assessment period.

## <span id="page-12-0"></span>*Femoral Artery Ligation*

To replicate the ischemic conditions associated with PAOD, a suture-based ligation was performed on the hindlimb of each subject. The ligation site was specifically targeted at the femoral artery, chosen as the region upstream (proximal) to the saphenous and popliteal arteries, and downstream (distal) from the epigastric and profunda arteries. Mice were first anesthetized in an induction chamber using a mixture of 5% isoflurane in oxygen, with a flow rate ranging from 0.8 to 1.6 L∙min-1 . Once adequately anesthetized, the mice were weighed and transferred to the preparation stage, where they were positioned in a supine

delivered through a 'nose-cone'. On the preparation bench, veterinary ophthalmic ointment was applied to the eyes to prevent corneal desiccation and depilatory cream was used to remove the hair from the surgical area on the medial aspect of both hindlimbs. Before placing the mouse on the surgical stage, a preoperative analgesic of buprenorphine (0.075 mg∙kg-1 ) was administered subcutaneously via injection. To maintain the body temperature of the mice at 35°C, a temperature-controlled heat pad, and a thermal rectal probe. All surgical instruments were autoclaved prior, and aseptic technique was maintained throughout the entirety of the surgical procedure to prevent contamination and wound infection.

orientation while receiving 1.5-2.5% isoflurane mixed with oxygen

Within the neurovascular bundle, the femoral artery was separated from the adjacent vein and nerve before ligating the vessel with 6.0



**Figure 4. Femoral Artery Ligation and Implantation.** Ligation tied at femoral artery 6.0 silk suture (A) followed by injection of thermally responsive polymer underneath the gracilis muscle (B).

silk suture (**Figure 4A**). A thermally responsive polymer with myoblasts (n=11, 2 lean and 9 DIO subjects) was injected underneath the gracilis muscle of the operated hindlimb (**Figure 4B**). The nontreated subjects were given cell-free polymer vehicles (n=11, 3 lean and 8 DIO subjects),. After implantation, the skin incision was closed using 7-0 polypropylene suture. As the control, a sham surgery was performed on the contralateral limb of each subject except for the neurovascular separation, femoral artery ligation, and polymer implantation. Buprenorphine was administered immediately post-operation (0.075 mg·kg-1 ), and the subject was contained in a recovery bin until ambulatory. Analgesic was given for two consecutive days after the day of operation.

## <span id="page-13-0"></span>*Perfusion Fixation and Vascular Casting*

Perfusion fixation and vascular casting were performed to prepare for immunofluorescent staining and imaging of the gracilis muscle collateral. First, a thoracotomy was done to achieve access to the heart, which was then cannulated using a 23G needle in the left ventricle. An incision in the right atrium of the heart was made prior to injecting 25ml of the vasodilator cocktail heated to 37 °C (5 U·µL<sup>-1</sup> heparin, 10<sup>-4</sup> M sodium nitroprusside,  $10^{-4}$  M adenosine, in phosphate buffer solution (PBS)) at about 5ml/min, followed by 4% paraformaldehyde injected at a pressure of 90-110 mmHg. Next, vascular casting was completed by injecting a microfilament solution at a rate of 0.5-0.9 ml/min using a syringe pump until the casting spanned the anterior gracilis collaterals **(Figure 5**).



**Figure 5. Vascular Casting.** The casting set-up entails the use of a syringe pump to inject the microfilament solution **(A)** into the subject's system through a cannula placed in the pre-existing hole in the left ventricle **(B)**. The infusion is stopped once the solution spreads through the gracilis anterior collateral **(C)**.

Once the solution surpassed the knee joint in the saphenous artery, a makeshift tourniquet, using 2.0 silk suture, was tied around the ankle to prevent the microfilament from entering the veins through the ankle A-V shunts. To allow time for the microfilament to cure, the subjects were left overnight at room temperature, and the gracilis muscles from the operated and sham hindlimbs were resected the following day. The anterior gracilis and the adjacent saphenous artery were stored in a microcentrifuge tube with PBS at 4°C before immunofluorescent staining.

## <span id="page-14-0"></span>*Immunofluorescence and Microscopy*

Immunofluorescence staining was carried out to visualize the smooth muscle surrounding the collateral. The gracilis anterior muscles were stained with α-smooth muscle actin (ASMA) in a solution containing 2% bovine serum albumin (BSA) and 0.1% Triton in PBS for approximately 72 hours at 4°C. After the staining period, the muscles were rinsed in 0.1% Triton in PBS three times for 10 minutes, in addition to a PBS rinse for 30 minutes at room temperature.

Images of the collaterals were obtained through an inverted widefield microscope, in parallel with the Infinity Capture imagining software. A fluorescence setting (Cy3 excitation: 550 nm, emission 570 nm) on the microscope was used to view and take photos of the ASMA stain at a 4X and 10X objective. The brightfield setting on the same microscope was set to observe the microfilament casting in the collateral lumen, and an image was captured at a 10X objective.

## <span id="page-14-1"></span>*Data Collection and Analysis*

All diameter measurements were taken from the 10X images using the line measuring tool in ImageJ software. The measurement scale was calibrated at 10X prior to taking the data of the collaterals. Measurements were taken at the midzone in three locations along the collateral. Outer (abluminal) vessel diameter was taken from the collateral width on the ASMA fluorescent images, the inner (luminal) vessel diameter was taken from the collateral width along the same zone on the vascular casting images. The arterial wall thickness was calculated from the inner and outer diameter measurements.

Differences in the inner and outer diameters, and collateral wall thicknesses among the various groups were determined through a two-way ANOVA and Tukey Post-Hoc comparisons. All values are expressed as mean  $\pm$  standard error.

## <span id="page-15-0"></span>RESULTS

The aim of this study was to develop a regenerative cell therapy for inducing natural bypass enlargement in patients with atherosclerotic arteries, a common occurrence in PAOD. To achieve this, ischemic conditions were created in the subjects by performing femoral artery ligation surgery (n=22), followed by the implantation of a thermally responsive, injectable polymer with  $(n=11)$  or without  $(n=11)$  myoblasts . After 7 days post-surgery, perfusion fixation and vascular casting techniques were employed to allow measurement of collateral diameters post with fluorescence and brightfield microscopy. In summary, myoblasts did not enhance the enlargement of collaterals in the gracilis anterior muscles (**Figures 6-8)**.

Myoblasts did not impact the luminal diameters of the collaterals in the anterior gracilis (**Figure 6**). There was no significant difference in the inner diameter on the operated hindlimb that received myoblasts between phenotypes (lean:  $65.0 \pm 3.12 \mu m$ , DIO:  $66.7 \pm 10.3 \mu m$ ), or between the operated hindlimbs that received the control vehicle (lean:  $67.3 \pm 21.5$ , DIO:  $74.23 \pm 4.94 \mu m$ , respectively).



**Figure 6. Luminal Diameter of Anterior Gracilis Collateral 7 Days Post-Artery Ligation and Implantation. (A)** Representative day-7 post ligation collateral luminal diameter Microfilament casted in sham hindlimb (10x). **(B)** Representative day-7 post ligation collateral luminal-diameter Microfilament casted in operated hindlimb (10x). **(C)** The inner diameters  $(\mu m)$  of anterior gracilis collaterals in day-7 post-ligation hindlimbs in DIO w/cell treatment, lean w/ cells, DIO w/o cells, and lean w/o cells (n=6, 2, 7, 3)\* and the control hindlimbs (sham) in DIO w/cell treatment, lean w/cells, DIO w/o cells, and lean w/o cells (n=8, 2, 7, 1)\* (all C57Bl/6 male mice). No differences were detected between the inner diameters of DIO and lean subjects or between mice that received the myoblasts or vehicle transplant. (\*n represents the number of hindlimbs, not subjects).

Likewise, myoblasts did not affect the abluminal diameters of the collaterals **(Figure 7)**, as the outer diameters in the operated hindlimb with the treatment (lean:  $72.84 \pm 4.85 \mu m$ , DIO:  $66 \pm 11.2 \mu m$ ) were not significantly different then in operated limbs with the control vehicle (lean:  $76.8 \pm 18$ ., DIO:  $81.77 \pm 7.35$ μm, respectively).



**Figure 7. Abluminal Diameter of Anterior Gracilis Collateral 7 Days Post-Artery Ligation and Implantation. (A)** Representative day-7 post ligation collateral abluminal diameter ASMA stained in sham hindlimb (10x). **(B)** Representative day-7 post ligation collateral abluminal-diameter ASMA stained in operated hindlimb  $(10x)$ . **(C)** The outer diameters  $(\mu m)$  of anterior gracilis collaterals in day-7 post-ligation hindlimbs in DIO w/cell treatment, lean w/cells, DIO w/o cells, and lean w/o cells  $(n = 9, 2, 8, 3)$ <sup>\*</sup> and the control hindlimbs (sham) in DIO w/cell treatment, lean w/cells, DIO w/o cells, and lean w/o cells (n = 8, 2, 8, 3)\* (all C57Bl/6 male mice). No differences were detected between the outer diameters of DIO and lean subjects or between mice that received the myoblasts or vehicle transplant. (\*n represents the number of

Although the myoblasts did not impact the collateral wall thickness in the operated hindlimb (lean: 7.84  $\pm$ 1.73μm, DIO: 15.88 ± 2.89 μm) as the measurements were similar to the subjects that received the vehicle (lean:  $9.42 \pm 3.55$ , DIO:  $13.60 \pm 1.99$  µm, respectively), the wall thickness was larger in mice with DIO than in lean mice (p<0.05) (**Figure 8**).



**Figure 8. Wall Thickness of Anterior Gracilis Collateral 7 Days Post-Artery Ligation and Implantation.** The arterial wall thickness ( $\mu$ m) of anterior gracilis collaterals in day-7 post-ligation hindlimbs in DIO w/cell treatment, lean w/ cells, DIO w/o cells, and lean w/o cells (n=6, 2, 7, 3)\* and the control hindlimbs (sham) in DIO w/cell treatment, lean w/cells, DIO w/o cells, and lean w/o cells (n=8, 2, 7, 1)\* (all C57Bl/6 male mice). The statistical analysis demonstrates that the wall thickness in DIO subjects is greater than in lean subjects ( $p<0.05$ ). However, there is no difference in arterial wall thickness between subjects that received the cell treatment and those that received the vehicle. (\*n represents the number of hindlimbs, not subjects).

## <span id="page-18-0"></span>DISCUSSION

Peripheral Arterial Occlusive Disease (PAOD) affects around 8-12 million individuals [24]. This condition arises when excessive cholesterol in the bloodstream accumulate as plaque in the arteries, leading to a reduction in blood flow to the limbs or other distant organs. While about 50% of people with this condition do not experience any symptoms, the disease can result in claudication and progress to a stage known as critical limb ischemia, which significantly increases the risk of limb amputation. In response to the mechanical pressures and stresses caused by arterial occlusion, the natural bypass arteries can enlarge through a process called arteriogenesis, which helps increase blood flow to the areas of

reduced perfusion. This study aimed to explore the potential of cell therapy, specifically the use of muscle progenitor cells known as myoblasts, to enhance the arteriogenesis process in cases of PAOD and analyze the treatment's effects on obese subjects. Mice with DIO and lean mice were surgically modified to mimic ischemic conditions found in patients of PAOD, and other in-vivo surgical procedures were utilized to investigate the effects of myoblast transplantation on arteriogenesis.

The data from this study concludes that myoblasts did not enhance nor impair arteriogenesis. In contrast to the previous study that utilized a gelatin vehicle and demonstrated significant outcomes with myoblast implantation, the present experiment employed a N-isopropylacrylamide (NIPAM) based polymer, which has shown to be a biocompatible vehicle for myoblasts [25]. In the NIPAM construct, the cells were dispersed throughout the material, while in the gelatin construct, the cells were primarily located on the top layer that was in direct contact with the gracilis upon implantation [23]. Therefore, one plausible theory for the non-replication of results in this study could be that an adequate number of myoblasts in the NIPAM vehicle could not migrate sufficiently close to the collaterals to induce a local response. Further investigations involving cell tracking in the polymer and local muscle fibers on the 7-day assessment are necessary to ascertain the impact of cell placement and migration within the polymer on collateral remodeling.

Mouse phenotype, i.e., diet induced obesity or lean did not impact the abluminal and luminal diameters of the anterior gracilis collaterals. As expected, there was greater collateral remodeling in the operated hindlimbs compared to the sham hindlimbs (Appendix I), ensuring that the femoral artery ligation was overall effective in mimicking the ischemic conditions found in patients with PAOD.

Although myoblast treatment had no effect, it was evident that the wall thickness in the subjects with DIO was larger than that in the lean subjects. A greater intima-media thickness has been repeatedly observed in the carotid arteries in obese humans, and a few studies even suggest that body weight has a greater impact on the arterial thickness relative to lumen diameter [26-28]. A greater wall thickness is indicative of vascular smooth muscle cell (VSMC) hypertrophy, which occurs in response to arterial

injury and remodeling, such as in cases of atherosclerosis [29]. This hypertrophic response is influenced by the interaction of VSMCs with endothelial cells, inflammatory cells, and a variety of growth factors. Patients with obese phenotypes often exhibit elevated levels of perivascular adipose tissue (PVAT), which directly surrounds blood vessels and exerts local effects on vascular function [30]. Growth factors released from the perivascular fat can regulate VSMC proliferation and migration from the tunica media to intima, leading to overall hypertrophic changes. Adipokines, including Visfatin, which are cytokines released by PVAT, partially induce VSMC hypertrophy through paracrine signaling and adipocyteconditioned media containing Visfatin derived from human adipocytes can increase the human VSMCs proliferation [30]. Moreover, PVAT adipocytes express and secrete significant amounts of growth factors such as thrombospondin-1, vascular endothelial growth factor (VEGF), and basic fibroblast growth factor (bFGF), which stimulate VSMC proliferation and migration [31]. Even though a majority of PVAT is located around arteries, large veins, and arterioles it can also be found within the vascular walls of small vessels located within striated muscle [32, 33]. If the mice with DIO in this study had higher levels of PVAT within the collateral vessels, the increased presence of adipokines and PVAT-derived growth factors could potentially explain the notable increase in wall thickness observed in the obese subjects.

The study encountered several limitations that should be taken into consideration. Firstly, it is important to note that the vascular casting procedure encountered difficulties in nine hindlimbs (two in the lean group and seven in the DIO group). The protocol failed in these subjects as the Microfilament solution did not reach the targeted collaterals, hence a luminal diameter measurement could not be obtained. Another limitation that may have affected the accuracy of the data is the blurriness observed in some of the ASMA fluorescent collateral images. In certain samples, the position of the collateral in relation to the surrounding muscles made it challenging to obtain a clearly defined outer diameter edge, thus posing difficulties in accurate measurement taking using ImageJ. The lack of well-defined edges could have introduced variability and potential measurement errors, which should be taken into consideration when interpreting the results.

Future studies should prioritize identifying the factors contributing to the failure of the vascular casting procedure to significantly improve the consistency and reliability of luminal diameter measurements. Perhaps preparing the stained muscle in a way that allows for clear capturing of images at 40X objective, as opposed to 10X, will yield to more precise data. Furthermore, to reduce variability, future studies should focus on maintaining a singular phenotype during the investigation by selecting either all lean or mice with DIO for studying the arteriogenic response to femoral artery ligation. The present study had a small sample size of only 5 lean mice compared to 17 mice with DIO. This discrepancy in sample sizes may have made it challenging to make a fair comparison between the outcomes of the two phenotypes, and instead, introduced unnecessary variability.

Given that the significant differences observed in this study were primarily related to wall thickness variations among phenotypes, it would be worthwhile to conduct a research study that measures collateral remodeling in both mice with DIO and lean mice without the myoblast transplantation. This approach would provide a clearer examination of the natural biochemical differences that occur, and such research could supplement our understanding of how regenerative solutions can enhance the arteriogenic response in both patient phenotypes.

## <span id="page-21-0"></span>**CONCLUSION**

The study findings demonstrated that myoblasts did not enhance arteriogenesis in mice with DIO. However, an interesting observation was made regarding the larger wall thickness of the collateral vessels in the obese subjects. This suggests the involvement of significant paracrine signaling of growth factors and cellular processes triggered by arterial occlusion, that are possibly present in greater quantities in obese individuals. To gain a deeper understanding of the myoblast treatment on arteriogenesis, further analysis should focus on studying it in a more balanced manner, either within a single phenotype or by ensuring a more equitable distribution of obese and lean subjects. The continued advancement of regenerative therapies offers the potential to provide alternative and minimally invasive treatments that

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can alleviate symptoms and improve overall patient outcomes. By harnessing the power of regenerative medicine, researchers can make significant strides in improving the lives of individuals affected by vascular diseases, including PAOD.

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## <span id="page-26-0"></span>**APPENDICIES**

## <span id="page-26-1"></span>*Appendix A: Raw Images*

(Absence of Microfilament images indicates that the Micofil solution did not enter the collateral during casting procedure.)

Replicate N1: Lean, Cell



Replicate N1: DIO, Cell



Operated

# Replicate N1: Lean, Vehicle



# Replicate N1: DIO, Vehicle



# Replicate N2: Lean, Cell



# Replicate N2: Lean, Vehicle



# Replicate N2: DIO, Vehicle



# Replicate N3: Lean, Cell



# Replicate N3: DIO, Cell



# Replicate N3: DIO, Vehicle



# Replicate N4: DIO, Cell



# Replicate N4: DIO, Vehicle



Replicate N5: DIO, Cell



Replicate N5: DIO, Vehicle



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# Replicate N6: DIO, Cell



# Replicate N6: DIO, Vehicle



# Replicate N7: DIO, Vehicle



## Replicate N7: DIO, Cell



Operated

# Replicate N8: DIO, Vehicle



# Replicate N8: DIO, Cell



# Replicate N9: DIO, Cell



# Replicate N10: DIO, Cell



# <span id="page-37-0"></span>*Appendix B: Raw Data*

ASMA Immunofluorescence (Outer Diameter) and Vascular Casting (Inner Diameter)





# <span id="page-39-0"></span>*Appendix C: Femoral Artery Ligation Protocol*



# <span id="page-40-0"></span>*Appendix D: Perfusion Fixation Protocol*



# <span id="page-41-0"></span>*Appendix E: Vascular Casting Protocol*



## <span id="page-42-0"></span>*Appendix F: ASMA Staining and Imaging Protocol*

## **Materials**

24-well culture plates (Cat#: 3738, Corning Incorporated) **PBS** 0.1% Saponin (Cat#: 47036, Sigma-Aldrich) 2% Bovine Serum Albumin (Cat# B6917, Sigma Aldrich) Monoclonal Anti-Alpha Smooth Muscle Actin, Cy3 Conjugate (Cat#: C6198, Sigma-Aldrich) **Slides** Coverslips Parafilm **Aluminum** foil

#### **Staining**

- 1. Using forceps, remove muscle from PBS (stored in microcentrifuge tube at  $4^{\circ}$ C) and place in a single well of a 24-well culture plate.
- 2. Prepare antibody solution containing 1:200 1A4 clone (alpha-smooth muscle actin, Cy3) conjugate) in 0.1% saponin (reconstituted in PBS), 2% BSA (reconstituted in PBS) in PBS, using 0.3mL of solution per muscle.
- 3. Incubate muscle in antibody solution for 3 nights (72 hours) at  $4^{\circ}$ C). (Note: Critical step-3 nights crucial for bright staining) by gently pipetting solution over muscle.)
- 4. Wash in 0.1% saponin in PBS 3x for 20 minutes at room temperature. Cover plate with foil during each wash.
- 5. Wash in plain PBS for 30 minutes. Cover with foil during each wash.
- 6. Place 1-2 drops of 50/50 PBS and Glycerol onto slide.
- 7. Remove muscle from well using forceps and place on a slide.
- 8. Add 1-2 drops of 50/50 PBS and Glycerol to the top of the muscle and place cover slips over the muscle.
- 9. Paint edges of coverslip with clear nail polish to create a seal and prevent tissue desiccation.
- 10. Store slides at 4°C wrapped in foil or an opaque container between imaging.

#### Imaging

11. Image using a standard fluorescent microscope. (Cy3 excitation: 550 nm, emission: 570 nm)

## <span id="page-43-0"></span>*Appendix G: Statistical Analysis*

Comparisons between Outer Diameter of Operated and Sham Hindlimbs

Analysis: Tukey Pairwise and 2-sample T-test

## **Tukey Pairwise Comparisons: Hindlimb**

## Grouping Information Using the Tukey Method and 95% Confidence

Hindlimb N Mean Grouping

Operated 22 73.8183 A Sham 22 43.4508 B

Means that do not share a letter are significantly different.

## WORKSHEET 6 Two-Sample T-Test and CI: Outer Diameter (um), Hindlimb

#### **Method**

µ<sub>1</sub>: population mean of Outer Diameter (µm) when Hindlimb = Operated µ<sub>2</sub>: population mean of Outer Diameter (µm) when Hindlimb = Sham Difference: µ1 - µ2

Equal variances are not assumed for this analysis.

#### Descriptive Statistics: Outer Diameter (µm)

Hindlimb N Mean StDev SE Mean

Operated 22 73.8 26.9 5.7 Sham 22 43.5 16.1  $3.4$ 

#### **Estimation for Difference**

95% CI for Difference Difference 30.37 (16.77, 43.97)

#### **Test**

Null hypothesis Ho: μ<sub>1</sub> - μ<sub>2</sub> = 0 Alternative hypothesis  $H_1$ :  $\mu_1$  -  $\mu_2 \neq 0$ 

T-Value DF P-Value

4.54 34 0.000

## Comparisons between Outer Diameter of Phenotype (DIO v. Lean) and Treatment (Cells v. Vehicle)

## Analysis: 2-way ANOVA and Tukey Pairwise

#### WORKSHEET 6 General Linear Model: Outer Diameter (µm) versus Phenotype, Treatment

#### **Method**

Factor coding (-1, 0, +1)

#### **Factor Information**

Factor Type Levels Values 2 DIO, Lean<br>2 Cells, Vehicle Phenotype Fixed Treatment Fixed

#### **Analysis of Variance**



#### **Model Summary**



#### **Coefficients**



#### **Regression Equation**

Outer Diameter (µm) = 57.80 + 1.73 Phenotype\_DIO - 1.73 Phenotype\_Lean

- 3.75 Treatment\_Cells + 3.75 Treatment\_Vehicle

- 1.17 Phenotype\*Treatment\_DIO Cells + 1.17 Phenotype\*Treatment\_DIO

- Vehicle + 1.17 Phenotype\*Treatment\_Lean Cells
- 1.17 Phenotype\*Treatment\_Lean Vehicle

## **Fits and Diagnostics for Unusual Observations**

Outer Diameter Obs (μm) Fit Resid Std Resid<br>8 125.6 54.6 71.0 2.67 R  $2.67R$ 

R Large residual









# Grouping Information Using the Tukey Method and 95% Confidence



Means that do not share a letter are significantly different.

## ('n' refers to number of hindlimbs, not subjects)



## Comparisons between Inner Diameter of Operated and Sham Hindlimbs

Analysis: Tukey Pairwise and 2-sample T-test

## ID Two-Sample T-Test and CI: Inner Diameter (µm), Hindlimb

#### **Method**

µ.: population mean of Inner Diameter (µm) when Hindlimb = Operated µ<sub>2</sub>: population mean of Inner Diameter (µm) when Hindlimb = Sham Difference: µ1 - µ2

Equal variances are not assumed for this analysis.

#### Descriptive Statistics: Inner Diameter (µm)

#### Hindlimb N Mean StDev SE Mean



#### **Estimation for Difference**

95% CI for Difference Difference 34.56 (22.42, 46.71)

#### **Test**

Null hypothesis  $H<sub>0</sub>: μ<sub>1</sub> - μ<sub>2</sub> = 0$ Alternative hypothesis H::  $\mu$ <sub>1</sub> -  $\mu$ <sub>2</sub>  $\neq$  0

#### T-Value DF P-Value

5.81 30 0.000

## **Tukey Pairwise Comparisons: Hindlimb**

## Grouping Information Using the Tukey Method and 95% Confidence

#### Hindlimb N Mean Grouping

Operated 18 69.5447 A Sham 18 34.9834 B

Means that do not share a letter are significantly different.

## Comparisons between Inner Diameter of Phenotype (DIO v. Lean) and Treatment (Cells v. Vehicle)

## Analysis: 2-way ANOVA and Tukey Pairwise

#### ID General Linear Model: Inner Diameter (µm) versus Phenotype, Treat

#### **Method**

Factor coding (-1, 0, +1)

#### **Factor Information**



#### **Analysis of Variance**



#### **Model Summary**



#### Coefficients



#### **Regression Equation**

Inner Diameter (µm) = 52.35 - 0.15 Phenotype\_DIO + 0.15 Phenotype\_Lean

- 6.07 Treatment\_Cells + 6.07 Treatment\_Vehicle

+ 1.19 Phenotype\*Treatment\_DIO Cells - 1.19 Phenotype\*Treatment\_DIO Vehicle - 1.19 Phenotype \*Treatment\_Lean Cells<br>+ 1.19 Phenotype \*Treatment\_Lean Cells<br>+ 1.19 Phenotype \*Treatment\_Lean Vehicle

#### **Fits and Diagnostics for Unusual Observations**



R Large residual









# Tukey Pairwise Comparisons: Phenotype\*Treatment

# Grouping Information Using the Tukey Method and 95% Confidence



Means that do not share a letter are significantly different.



## Comparisons between Wall Thickness of Operated and Sham Hindlimbs

Analysis: Tukey Pairwise and 2-sample T-test

## **Tukey Pairwise Comparisons: Hindlimb**

## Grouping Information Using the Tukey Method and 95% Confidence

Hindlimb N Mean Grouping Operated 18 13.0261 A Sham 18 11.3365 A

Means that do not share a letter are significantly different.



**WALL THICKNESS** 

# Two-Sample T-Test and CI: Wall Thickness (µm), Hindlimb

# **Method**

µ.: population mean of Wall Thickness (µm) when Hindlimb = Operated µ2: population mean of Wall Thickness (µm) when Hindlimb = Sham Difference: µ1 - µ2

Equal variances are not assumed for this analysis.

# Descriptive Statistics: Wall Thickness (µm)





# **Estimation for Difference**

95% CI for Difference Difference 1.69 (-1.88, 5.26)

## **Test**

Null hypothesis Ho:  $\mu_1 - \mu_2 = 0$ Alternative hypothesis H<sub>1</sub>: µ<sub>1</sub> - µ<sub>2</sub> ≠ 0

T-Value DF P-Value 0.97 29 0.341

## Comparisons between Wall Thickness of Phenotype (DIO v. Lean) and Treatment (Cells v. Vehicle)

Analysis: 2-way ANOVA and Tukey Pairwise

## WALL THICKNESS

General Linear Model: Wall Thickness (um) versus Phenotype, Treatment

#### **Method**

Factor coding  $(-1, 0, +1)$ 

#### **Factor Information**



#### **Analysis of Variance**



#### **Model Summary**



## **Coefficients**



#### **Regression Equation**

Wall Thickness (µm) = 11.00 + 2.12 Phenotype\_DIO - 2.12 Phenotype\_Lean

- 0.13 Treatment\_Cells + 0.13 Treatment\_Vehicle

+ 0.50 Phenotype\*Treatment\_DIO Cells - 0.50 Phenotype\*Treatment\_DIO

Vehicle - 0.50 Phenotype\*Treatment\_Lean Cells

+ 0.50 Phenotype\*Treatment\_Lean Vehicle

#### **Fits and Diagnostics for Unusual Observations**

Wall Thickness (µm) Fit Resid Std Resid Obs 23.97 13.50 10.47 2.12 R  $\overline{2}$ 

R Large residual









#### Tukey Pairwise Comparisons: Phenotype\*Treatment

#### Grouping Information Using the Tukey Method and 95% Confidence



Means that do not share a letter are significantly different.

