



CAL POLY

Final Report Spring 2020

Septal Closure Device

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Executive Summary

The septal closure device was designed to seal defects in the atrial septum. To fully seal an atrial defect, the device was designed to consist of two circular seals to cover the defect in both the right and left atria, attached with a central rod. The materials were chosen for compressibility (for ease of insertion), biocompatibility, and tissue ingrowth. A CAD model was drafted in SolidWorks. Key customer requirements include ease of implantation (specifications: adjustable sizing and clear directions for use), physician controlled (specifications: short implantation time and compatibility with current catheter/scope techniques), and a long lifetime (specifications: materials that will not excessively degrade over time and material will become ingrown in endothelium). Key data that demonstrates functionality is plastic deformation not exceeding 1 mm after 2E9 cycles, no adverse reactions with the native tissue, and becoming ingrown with the native tissue.

Statement of Work

I. EXECUTIVE SUMMARY

This Statement of Work outlines the prevalence of need for a septal closure device and the current products available. The objectives for the new product are described and the plan for product development is described.

II. INTRODUCTION / BACKGROUND

200,000 cases of atrial septal defects are diagnosed in the United States every year [1]. An atrial septal defect occurs when the foramen ovale fails to close after birth. This results in deoxygenated blood in the patient, as blood continues to bypass the lungs after birth. There are multiple devices currently on the market to treat these defects, such as the Amplatzer septal occluder (ASO), Figulla Flexible Occlutech septal occluder (FSO), and many other similar devices [2]. Current devices come with possible complications, such as thrombus formation, air embolization, device embolization, erosions, residual shunts, and nickel hypersensitivity. The issue of septal defects will continue to need to be treated; as a result, new and improved techniques and devices need to be developed.

III. OBJECTIVES

The septal closure device aims to provide a way to close the atrial septum of the heart in patients recovering from septal crossing procedures and/or suffering from atrial septal birth defects. The device should be able to be controlled by physicians throughout the implantation procedure, and be easy to use and understand. The implant post implantation should demonstrate effectiveness in preventing blood from overfilling in the lungs and heart. The device should be able to become ingrown in the endothelium tissue.

IV. PROJECT MANAGEMENT

This project will be managed by the three team members: Kai Harrison, Hillal Jarrar, and Olivia Welch. A plan and schedule has been implemented in order for the project to stay on track and to allow certain deadlines to be met. The schedule will be followed in order to complete the project in the time allotted (two quarters). Dr. Whitt will be a source of guidance while moving through the design process.

V. CONCLUSION

The aim of this project is to develop a septal closure device that is controllable by physicians during implantation and becomes ingrown in the endothelium tissue. This Statement of Work will be followed by an analysis of quality specifications with the House of Quality and with the conjoint analysis, later this week. A project planning meeting will be conducted with Dr. Whitt, next week.

VI. REFERENCES / WORKS CITED

[1] "Atrial Septal Defect (ASD)," *Mayo Clinic*, 2020.

[2] N. Bissessor, "Current perspectives in percutaneous atrial septal defect closure devices," *Medical Devices, Auckland*, July 15, 2015.

VII. APPENDICES

Design Requirements:

1. Time to Implantation
2. Lifetime
3. Biocompatibility/Thrombogenicity

Indications for Use

The septal closure device is indicated for relief of an opening in the atrial septum in patients recovering from septal crossing procedures and/or who are born with septal defects. Qualifying patients are examined by a team of physicians, including a cardiovascular surgeon, to be determined fit for the device.

The septal closure device is indicated for use in patients in need of a closure in the atrial septum, either from the effects of surgery or atrial septal defects.

Network Diagram

- This project is planned over the span of two quarters

Task Mode	Task Name	Duration	Start	Finish	Predecessors
	Background Research	5 days	Tue 1/21/20	Mon 1/27/20	
	Heart Research	2 days	Tue 1/21/20	Wed 1/22/20	
	Existing Products	3 days	Thu 1/23/20	Mon 1/27/20	2
	Budget				
	Summary #1 Complete	0 days	Mon 1/27/20	Mon 1/27/20	3
	Material Selection	7 days	Tue 1/28/20	Wed 2/5/20	
	Material Research	6 days	Tue 1/28/20	Tue 2/4/20	5
	Material Selection	1 day	Wed 2/5/20	Wed 2/5/20	
	Summary #2 Complete	0 days	Tue 2/4/20	Tue 2/4/20	7
	Design	14 days	Thu 2/6/20	Tue 2/25/20	
	Concept sketches	4 days	Thu 2/6/20	Tue 2/11/20	
	Concept selection	2 days	Wed 2/12/20	Thu 2/13/20	11
	3D modeling	8 days	Fri 2/14/20	Tue 2/25/20	12
	Summary #3 Complete	0 days	Tue 2/25/20	Tue 2/25/20	
	Prototyping	47 days	Wed 2/26/20	Thu 4/30/20	
	Detailed drawing(s)	7 days	Wed 2/26/20	Thu 3/5/20	
	Ordering materials	14 days	Fri 3/6/20	Wed 3/25/20	16
	Contact manufacturers	14 days	Fri 3/6/20	Wed 3/25/20	
	Rapid prototyping	10 days	Thu 3/26/20	Wed 4/8/20	18
	Prototype testing & review	7 days	Thu 4/9/20	Fri 4/17/20	19
	Final product manufacturing	7 days	Mon 4/20/20	Tue 4/28/20	20
	Report	21 days	Wed 4/29/20	Wed 5/27/20	
	Written report	14 days	Wed 4/29/20	Mon 5/18/20	
	Presentation preparation	7 days	Tue 5/19/20	Wed 5/27/20	23

Figure 1. Network diagram from Microsoft project

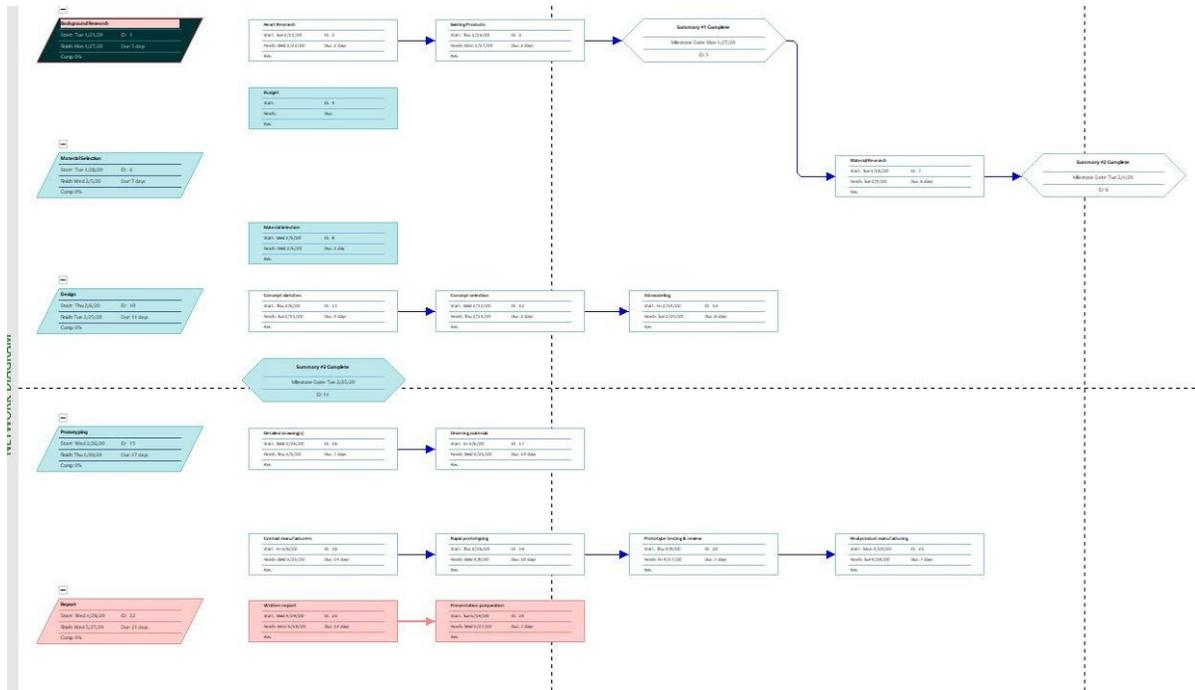


Figure 2. Network Diagram

Project Plan Modifications:

Nitinol scaffolding will be prototyped in week one of Spring quarter. The original plan was to prototype the scaffolding with a more available metal such as aluminum or steel. However, the Hannah-Forbes Fund will make a more advanced prototype possible.

Reconduct conjoint analysis through Abbott connection. If we are given the opportunity to work with an engineer from Abbott, we may have the ability to conduct the conjoint analysis with cardiologists, in order to obtain meaningful results.

Budget

Item Description	Purpose	
Materials		Prototyping
Nitinol		\$45
PTFE		\$30
Metal to Metal Epoxy (non-medical grade)		\$5
LOCTITE Adhesive and Glue (non-medical grade)		\$20
	Total Material Cost	\$100
Manufacturing Costs		Prototyping/Final Product
		\$600
	Total Manufacturing Cost	\$600
Testing		
		\$0
	Total Testing Costs	\$0
		\$700

Figure 3. Budget spreadsheet for septal closure device taken from Microsoft Excel

Modifications:

The following prices of scaffolding and tissue integrator materials were obtained:

- Nitinol Scaffolding- 14.99 USD per 5 feet of 1 millimeter diameter wiring (amazon.com)
- PTFE Tissue Integrator- 4.70 USD per 9 square feet (eplastics.com)

Customer Requirements/Specification Development

Table 1. Engineering Specifications

Factor	Specification 1	Specification 2
Easy Implantation	Adjustable sizing	Straight forward directions for use
Physician Controlled	Short implantation time	Compatible with current catheter/scope techniques
Long Lifetime	Materials that will not excessively degrade over time	Material will become ingrown in endothelium

Table 2. Customer Requirements related to engineering specification

Customer Requirements	Engineering Specs/Testing
Device Lifetime	Stress Failure and Biocompatibility Testing
Cost	Materials and Manufacturing Cost Analyses
Growth Compatibility	Rate/Percent of Encapsulation By Myocardial Tissue

Table 3. Engineering Specifications Targets and Importance

Engineering Specs	Targets and Importance
Stress Failure	Must Withstand 40mmHg Pressure for simulated 100 years
Cost	Target: \leq \$250 per unit
Growth Compatibility	Target: \geq 75% encapsulation

TAM and Competitive Advantage

The global revenue for atrial septum closure devices is estimated to be about \$93M (Marketwatch.com). The global average device cost is about \$8000 (USD) (Marketwatch.com). Based on these statistics and the estimated prices of our device, our annual revenue is estimated to be about \$2.9M assuming total control of the global market. After researching existing products, we came to the realization that our price estimates are grossly undervalued compared to the existing market and we will be revisiting the financial projections of our device.

Modifications: A recent report from Marketwatch.com indicates that the market is currently valued at \$600 million and will reach \$1.2 billion by 2025.

Intellectual Property Assignment

Three issued patents:

- 1. Methods and systems for endovascularly clipping and repairing lumen and tissue defects**
 - a. Pulsar Vascular, Inc.

Potential Patent Infringements:

- A delivery system incorporating an implantable device for repairing an opening or cavity in a target tissue defect, comprising: a delivery catheter comprising a distal end for delivery to a site in proximity to a target tissue defect; an implantable device slidably disposed in the delivery

<http://patft.uspto.gov/netacgi/nph-Parser?Sect1=PTO2&Sect2=HITOFF&p=1&u=%2Fmetahtml%2FPTO%2Fsearch-bool.html&r=2&f=G&l=50&co1=AND&d=PTXT&s1=%22septal+closure%22&OS=%22septal+closure%22&RS=%22septal+closure%22>

3. Patent foramen ovale (PFO) closure device with linearly elongating petals

a. W.L. Gore & Associates Inc.

Potential Patent Infringements:

A device for occluding a defect in a body, the occluder comprising: an occluder body that is reconfigurable between an elongated tubular cylindrical delivery configuration and a shortened deployed configuration, the occluder body comprising a plurality of filaments, each filament of the plurality of filaments comprising (i) a proximal end portion, (ii) a distal end portion, (iii) a central portion disposed between the proximal end portion and the distal end portion, (iv) a proximal free segment disposed between the proximal end portion and the central portion, and (v) a distal free segment disposed between the central portion and the distal end portion, the proximal end portion of each filament of the plurality of filaments being bonded together and aligned to form the proximal end portion and defining a generally tubular cylindrically shaped joint, the central portion of each filament of the plurality of filaments being bonded together and aligned to form the central portion and defining a generally tubular cylindrically shaped joint, and the distal end portion of each filament of the plurality of filaments being bonded together and aligned to form the distal end portion and defining a generally tubular cylindrically shaped joint, wherein, when the occluder body is in the deployed configuration, the proximal free segment of each filament of the plurality of filaments forms a proximal loop, and the distal free segment of each filament of the plurality of filaments forms a distal loop, wherein each of the proximal loops of each filament of the plurality of filaments overlaps with adjacent proximal loops of the plurality of filaments at a discrete location within an occlusive proximal face formed by the proximal loops, wherein each of the distal loops of each filament of the plurality of filaments overlaps with adjacent distal loops of the plurality of filaments at a discrete location within an occlusive distal face formed by the distal loops, wherein the occlusive distal face and the occlusive proximal face cooperate to occlude the defect and wherein each filament of the plurality of filaments comprises a discrete wire.

- The device of claim 1, wherein a first filament of the plurality of filaments has a semi-circular cross-section.
 - To avoid a patent infringement, design device so that the plurality of filaments does not have a semi-circular cross-section
- The device of claim 1, wherein, when the occluder body is in the deployed configuration, each of:
 - (a) the proximal end portion, (b) the central portion, and (c) the distal end portion are generally coaxially aligned with a longitudinal axis of the occluder body.
 - To avoid a patent infringement, design device to be reversible and not have a proximal end portion and distal end portion

- The device of claim 1, wherein a first filament of the plurality of filaments is coated with a therapeutic agent.
 - To avoid patent infringement, coat filaments with a different therapeutic agent.

Three patent applications:

1. *Trans-Septal Closure Device*

- a. Edwards Lifesciences

Potential Patent Infringements:

- “An implantable closure device comprising: a self-expanding metal frame comprising a central portion defining a lumen and a plurality of first anchoring arms and a plurality of second anchoring arms angularly spaced around the central portion;”
 - Use a different general design and different material

<http://appft.uspto.gov/netacgi/nph-Parser?Sect1=PTO2&Sect2=HITOFF&p=1&u=%2Fnethtml%2FPTO%2Fsearch-bool.html&r=45&f=G&l=50&co1=AND&d=PG01&s1=septal&s2=closure&OS=septal+AND+closure&RS=septal+AND+closure>

2. *Catheter Atrial Septal Closure Device*

- a. TAVR Solutions, LLC

Potential Patent Infringements:

- “An apparatus for occluding a bodily passageway, the apparatus comprising: a structure comprising a shape-memory metal alloy; and a membranous material attached to the structure; wherein the structure is adapted to be deployed adjacent to the bodily passageway; wherein the structure is adapted to sealingly engage the bodily passageway.”
 - Use a different material and a possible different technique for the device to attach to the endothelium (this patent is very general as it isn’t specific to the heart only)
- ...”wherein the securing region defined by the occlusion device sealing engages the bodily passageway.”
 - Be very specific with how our device will become in-grown with the endothelium

<http://appft.uspto.gov/netacgi/nph-Parser?Sect1=PTO2&Sect2=HITOFF&p=2&u=%2Fnethtml%2FPTO%2Fsearch-bool.html&r=53&f=G&l=50&co1=AND&d=PG01&s1=septal&s2=closure&OS=septal+AND+closure&RS=septal+AND+closure>

Card #	Cost	Lifetime	Time to Implantation	Level 1=0	Level 2=1	Card 1	Card 2	Card 3	Card 4	Cost	Lifetime	Time to Implantation
2	3	0	1	1								
3	2	1	1	1								
4	4	1	0	0								
5	1	0	0	0								
6	3	0	1	1								
7	2	1	1	1								
8	1	0	0	0								
9	4	1	0	0								
10	3	0	1	1								
11	2	1	1	1								
12	1	0	0	0								
13	4	1	0	0								
14	3	0	1	1								
15	2	1	1	1								
16	1	0	0	0								
17	4	1	0	0								
18	1	0	0	0								
19	3	0	1	1								
20	4	1	0	0								
21	2	1	1	1								
22	1	0	0	0								
23	3	0	1	1								
24	4	1	0	0								
25	2	1	1	1								
26	3	0	1	1								
27	2	1	1	1								
28	1	0	0	0								
29	4	1	0	0								
30	3	0	1	1								
31	2	1	1	1								
32	1	0	0	0								
33	4	1	0	0								
34	3	0	1	1								
35	2	1	1	1								
36	1	0	0	0								
37	4	1	0	0								

Figure 6. Data input for conjoint analysis

SUMMARY OUTPUT								
<i>Regression Statistics</i>								
Multiple R	0.4472136							
R Square	0.2							
Adjusted R Square	0.12121212							
Standard Error	1.04446594							
Observations	36							
<i>ANOVA</i>								
	<i>df</i>	<i>SS</i>	<i>MS</i>	<i>F</i>	<i>Significance F</i>			
Regression	3	9	3	4.125	0.01397487			
Residual	33	36	1.09090909					
Total	36	45						
	<i>Coefficients</i>	<i>Standard Error</i>	<i>t Stat</i>	<i>P-value</i>	<i>Lower 95%</i>	<i>Upper 95%</i>	<i>Lower 95.0%</i>	<i>Upper 95.0%</i>
Intercept	2	0.301511345	6.63324958	1.515E-07	1.38657056	2.61342944	1.38657056	2.61342944
X Variable 1	1	0.348155312	2.87228132	0.00707001	0.29167269	1.70832731	0.29167269	1.70832731
X Variable 2	-2.591E-16	0.348155312	-7.441E-16	1	-0.7083273	0.70832731	-0.7083273	0.70832731
X Variable 3	0	0	65535	#NUM!	0	0	0	0

Figure 7. Data output and results from conjoint analysis

Morphology

Morphology						
Product: Septal Closure Device		Organization Name: Septal Closure Device Team - BMED 455				
Function	Concept 1	Concept 2	Concept 3	Concept 4	Concept 5	Concept 6
Tissue ingrown	Polytetrafluoroethylene (PTFE) patch	PLGA poly(lactic-co-glycolic acid) patch	Bovine Pericardium	PTFE with anti infection treatment	PLGA poly(lactic-co-glycolic acid) patch with Anti infection Treatment	Bovine Pericardium with anti infection treatment
Scaffolding / strength	PLGA poly(lactic-co-glycolic acid) - scaffolding within patch (10 rungs)	PLGA poly(lactic-co-glycolic acid) - scaffolding within patch (4 rungs)	Nitinol - scaffolding within patch (10 rungs)	Nitinol - scaffolding within patch (4 rungs)	PLGA poly(lactic-co-glycolic acid) -scaffolding connecting two patches	Nitinol - scaffolding connecting two patches
Anti Infection	Taurolidine-Citrate Solution (TCS) treatment	Thermafix treatment	Microban Anti-microbial Polymer coating	chlorohexedine impregnation into external surface		
Geometry	Square (cover septum on one side)	Circular (cover septum on one side)	Double Square (cover septum on two sides)			
Team member: Hihal Jarrar		Team member: Olivia Welch		Prepared by: Septal Closure Device Team		
Team member: Kai Harrison		Team member:		Checked by: Septal Closure Device Team		Approved by:
The Mechanical Design Process Designed by Professor David G. Ullman Copyright 2008, McGraw Hill Form # 15.0						

Concept 1		Concept 1	Concept 2	Concept 3					
Function									
Tissue Ingrown	25	Datum		0	-1				
Scaffolding/strength	35			-1	1				
Anti infection	25			-1	0				
Geometry	15			1	-1				
			Total		-1	-1			
		Weighted Total		-45	-5				
Concept 2		Concept 2	Concept 1	Concept 3					
Function									
Tissue Ingrown	25	Datum		0	-1				
Scaffolding/strength	35			1	-1				
Anti infection	25			1	1				
Geometry	15			-1	1				
			Total		1	2			
		Weighted Total		45	50				
Concept 3		Concept 3	Concept 1	Concept 2					
Function									
Tissue Ingrown	25	Datum		1	-1				
Scaffolding/strength	35			-1	-1				
Anti infection	25			0	-1				
Geometry	15			1	-1				
			Total		1	-2			
		Weighted Total		5	-50				

After conducting the analysis through the Pugh Chart, we decided to choose concept one. Concept one has a circular shape geometry, and will cover the septum of the heart on one side. The material used for scaffolding is PLGA, and there will be 10 rungs of scaffold located on the patch. The patch itself will be made from Polytetrafluoroethylene (PTFE) in order for it to become ingrown in the tissue, and a Taurolidine-Citrate Solution (TCS) treatment will be added to help prevent infection after the device is implanted. Based on our analysis, these factors seem to be the best options for our design moving forward.

Conceptual Evaluation

Design Organization: Septal Closure Device Team

Date: 02/19/2020

Technology Being Evaluated: Septal Closure Device scaffolding and tissue integration

Table 4. Possible failures of different materials

Parameter	Function	Possible Failures
Nitinol	Scaffolding	Biocompatibility issues <ul style="list-style-type: none"> • Can release nickel ions into the body [1]
PLGA	Scaffolding	Softening <ul style="list-style-type: none"> • Studies showed that PLGA softened in wet environment versus dry environment [2]
PTFE	Tissue Integration	Negative Immune Response <ul style="list-style-type: none"> • Thrombosis [3] • Infection
PLGA	Tissue Integration	Negative Immune Response <ul style="list-style-type: none"> • Infection • May degrade too quickly [2]
Taurolidine-Citrate Solution (TCS)	Anti-infection	Anti-Infection Properties <ul style="list-style-type: none"> • May fail to prevent infection or lead to different type of infection

Current products that exist that demonstrate above qualities:

Nitinol:

- Stents
- Heart valve tools
- Septal Defect devices

Nitinol is already a common biomaterial used when developing septal defect devices.

Examples:

Amplatzer septal occluder (ASO): “The device structure is a self-expanding double disk with larger left atrial disk and a starting size 4 mm connector waist. The structure is a nitinol metal wire mesh framework and is recapturable...” [4]

Gore Helix septal occluder: “The device consists of a corkscrew type nitinol wire frame covered by a protective Gore-Tex (expanded polytetrafluoroethylene) coating...” [4]

PLGA (scaffold):

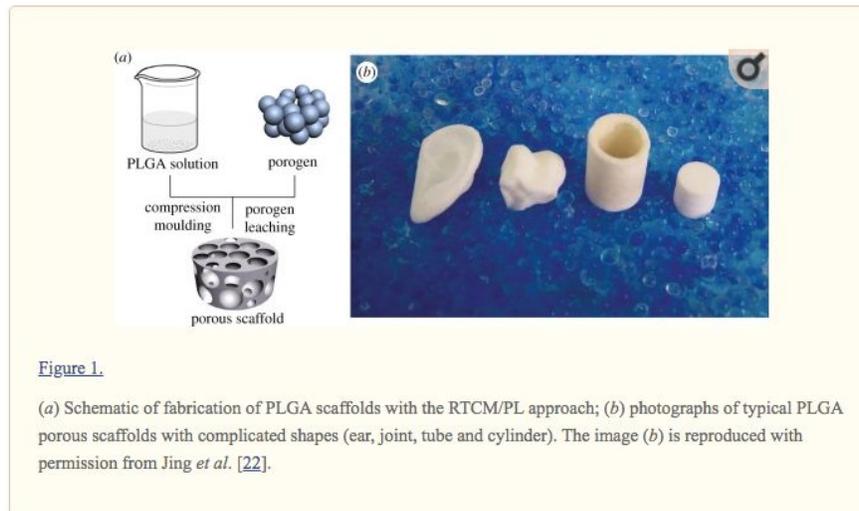


Figure 8. Example of PLGA scaffolding techniques taken from article [2] cited in references.

PTFE:

- Shunts
- Valve repair
- Vascular grafts
- Atrial septal defects

PLGA (tissue integrator):

- Used in current septal closure defects

“The sealing capability of biodegradable occluders was found superior to that of Amplatzer occluders. In addition, the cell attachment and spreading of endothelial cells seeded on the PLGA/collagen nanofibrous matrix and the interaction between cells and PLGA/collagen nanofibers were studied. The nanofibrous membranes made of PLGA/collagen were very effective in promoting cell proliferation during culture.” [5]

TCS:

- Used to aid in the prevention of central-line associated bloodstream infections
 - Study done in paediatric haematology-oncology and gastrointestinal failure patients with high baseline central-line associated bloodstream infection rates [6]

- “TCS usage was highly successful in CLABSI reduction by 80% in all patients, 90% in H/O and 70% in GI patients. In patients with high baseline CLABSI rates, TCS is an effective catheter-lock therapy to reduce CLABSI rates in paediatric patients.” [6]

Final Analysis

Based on our analysis, we believe that nitinol is the best choice for the scaffolding, PTFE as the tissue integrator, and Taurolidine-Citrate Solution (TCS) as the anti-infection agent. Based on our research of many different material options, these three choices overall follow our basic ideas and specifications we want in our design. This data was collected by using a modified version of the Technology Readiness Assessment, where we looked at different factors that were important to us in our design, and how different materials would affect these specifications. The specifications we looked at, as they are the main components of our design, were the scaffolding, the tissue integration, and the anti-infection agent.

For scaffolding, the two materials we were considering were nitinol and PLGA. Based on the technology readiness assessment, as well as some of our past research, nitinol seems to be the best choice moving forward. Nitinol has been used in septal closure devices previously, and has proven to be a reliable biomaterial when used in this aspect.

For the tissue integration aspect of our design, we want the device to be able to become integrated within the heart tissue. This will allow the device to function better as part of the body, and also promote cell growth to the damaged area, (atrial septal defect). Based on our analysis, we believe that PTFE is the best choice to use as the tissue integrator aspect of our device. PTFE has also been used previously in atrial septal defect devices.

Another important aspect of our design is the anti-infection agent. If a device is placed and an infection arises, that will lead to more surgery, which is not ideal for the physician or the patient. Including some sort of anti-infection agent within our device may help prevent unnecessary surgeries post implantation. The agent we chose to include within our device is Taurolidine-Citrate Solution (TCS), which is used to aid in the prevention of certain infections. Studies have been done showing that TCS can help prevent central line associated bloodstream infections, as well as infections that may result from the use of a catheter in certain procedures. Our device will likely be implanted using a catheter technique, so we believe using TCS as an anti-infection agent is the best choice.

The technology readiness assessment will help us move forward in our design, as we have mostly solidified our material selection. One of our next steps is to finalize our physical design, as well as develop a prototype that allows us to fully understand how our device will work.

Design Comments

Our first conceptual model (besides sketches) was done on SolidWorks. Based on our past analysis, our design is a circle with scaffolding coming from the middle. The circle (disk) will include the tissue integrator (PTFE) and the anti-infection agent (Taurolidine-Citrate Solution (TCS)). The

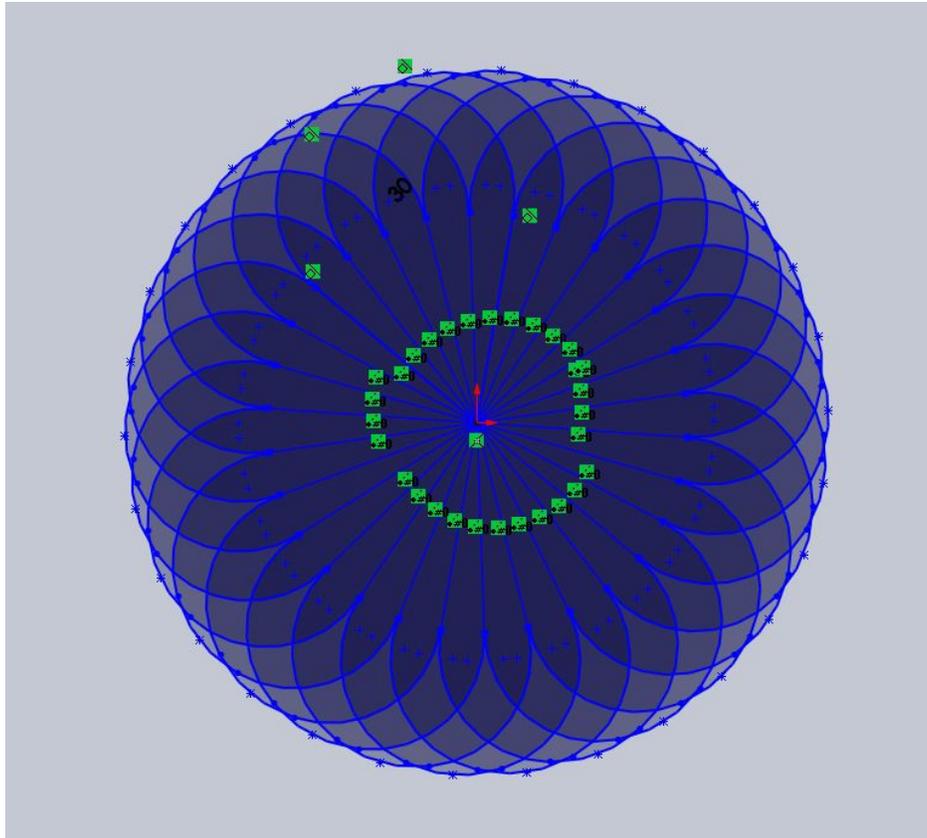


Figure 10. SolidWorks basic model of second design of septal closure device

Detailed Design

- Septal defects are classified into simple and complex defects
 - Simple: 4-26 mm diameter
 - Complex: >26 mm diameter
- Our device will be able to be adjusted to cover any size defect
 1. 8 mm diameter
 2. 12 mm diameter
 3. 18 mm diameter
 4. 24 mm diameter
 5. 28 mm diameter
- This will allow for the device to work for all sized defects
- We chose a two patch design in order to maximize the effectiveness of our device (our prior analysis showed we would be using a single patch design)

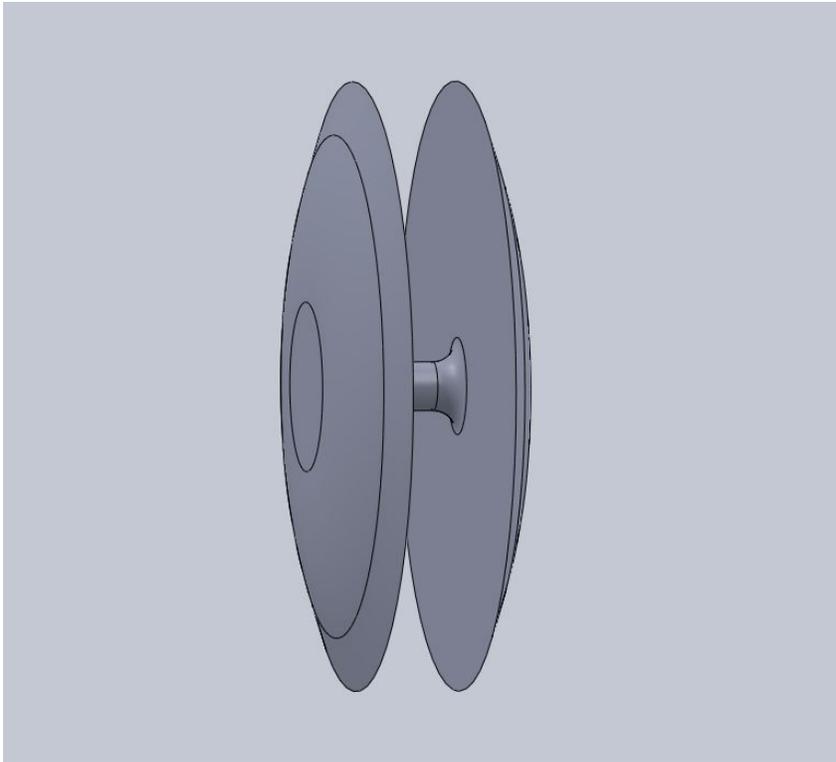


Figure 11. Solidworks design depicting full device

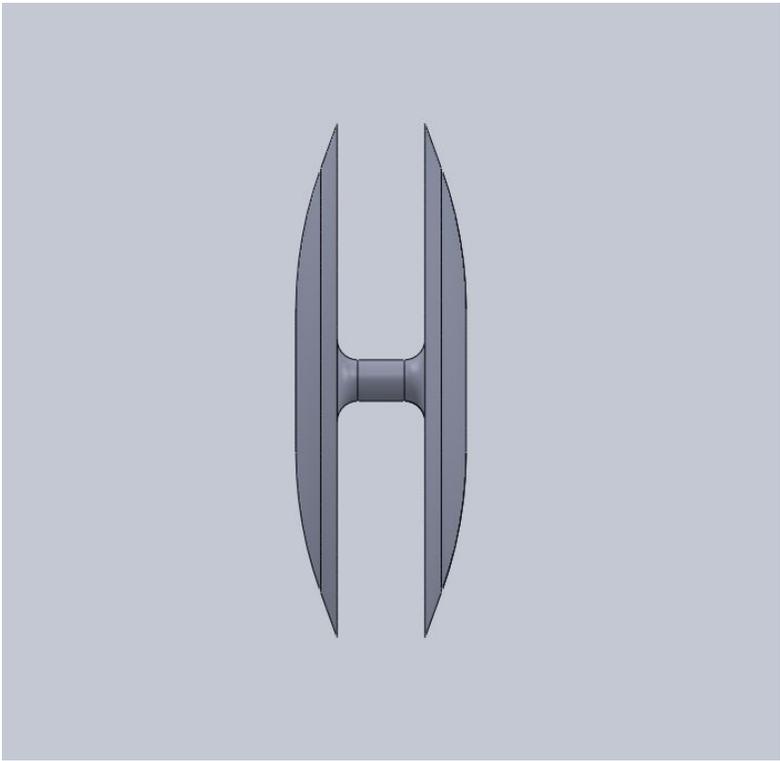


Figure 12. Side view

Prototype Manufacturing Plans

- We will develop a prototype to better understand how the scaffolding will sit inside the patch
- Prototype will be scaled up from actual dimensions
 - Nitinol
 - PTFE
 - Metal to metal epoxy (non-medical grade)
- Prototyping will take place mostly in 192-328
 - Nitinol wiring will require no tools (most likely) to bend
 - PTFE will be able to be cut with scissors
- Will use Mustang 60 if more equipment required
- Anti-infection agent will not be included in physical prototype

*Manufacturing was unable to take place due to COVID-19.

- Further information on this is examined in the Discussion section of this report

Test Plans

- Our device should have a lifetime of 50-100 years
 - Want to limit the need for secondary surgery to replace the device
 - Tissue ingrown
- Simulations will be run in COMSOL to test lifetime and durability of device
 - Simulations of 50 years, 75 years, 100 years
 - To better understand how wear in a beating heart will affect device
- Design will continue to be updated in SolidWorks as testing begins

Testing Data and Analysis

- Testing was unable to be completed due the current virtual classroom as a result of COVID-19.
 - Further information on this is examined in the Discussion section of this report

Conclusions

The septal closure device aims to provide a way to close the atrial septum of the heart in patients recovering from septal crossing procedures and/or suffering from atrial septal birth defects. The device should be able to be controlled by physicians throughout the implantation procedure, and be easy to use

and understand. The implant post implantation should demonstrate effectiveness in preventing blood from overfilling in the lungs and heart. The device should be able to become ingrown in the endothelium tissue. The device was designed with these ideas in mind, and engineering specifications were developed in order to achieve these goals.

This project was managed by three team members: Kai Harrison, Hillal Jarrar, and Olivia Welch. The team reported directly to Dr. Michael Whitt, and followed the implemented schedule to the best of their abilities. The project was completed over the span of two quarters.

As mentioned above the septal closure device is indicated for relief of an opening in the atrial septum in patients recovering from septal crossing procedures and/or who are born with septal defects. One of the first steps of the project included developing engineering specifications, which are based off the following factors:

- Easy implantation
- Physician controlled
- Long lifetime

The specifications related to easy implantation include the device having adjustable sizing and straight forward directions for use. In order to be physician controlled, the device will have a short implantation time and be compatible with current catheter/scope techniques. To provide a long device lifetime, the chosen materials will not excessively degrade over time, as well as become ingrown in the endothelium. These specifications were able to be met based on testing and analysis throughout the project. These specifications are shown in Table 1.

We also focused on the customer requirements of the device, which included device lifetime, cost, and growth compatibility. The device lifetime was/will be analyzed by stress failure and biocompatibility testing. The cost was analyzed by a materials and manufacturing cost analysis. The growth compatibility was/will be specified by the rate/percent of encapsulation by myocardial tissue. The targets and importance of these factors can be viewed in Table 3.

The team also analyzed other devices on the market, in order to determine other intellectual properties and avoid copyright infringements. These current devices on the market, from Pulsar Vascular, W.L Gore and Associates, Edwards Lifesciences, and TAVR Solutions were researched in order to better understand what is presently available to the consumer.

A conjoint analysis was also run in order to better understand what factors are most important to the customer. The statistical test was run using data from other students in BMED-456 (n=9). The factors included in the test were cost, lifetime, and time to implantation. The test showed to be somewhat inconclusive, as the students in senior design are not the device's intended customers.

The morphology of the device was analyzed, and a pugh chart was used in order to determine the best design for the device. This analysis can be seen in the *Morphology* section of this report. Based on the morphology assessment, the device was planned to be:

- Circular, one patch
- PLGA scaffolding
- PTFE patch
- TCS anti-infection agent

As our report shows, more testing proved that this was not the best design for the device. After conducting further analysis, slight changes were made to the morphology of the device.

A FMEA was conducted in order to officially choose the best materials for our device. After this test, the device's morphology was changed to better reflect our design specifications. The final design and morphology included

- Circular, two patch geometry
- Nitinol scaffolding
- PTFE patches
- TCS anti-infection agent

The designs of the septal closure device can be seen in Figures 9-12. The device will be able to be manufactured in multiple different sizes, in order to cover any size defect.

As a result of COVID-19, prototype manufacturing and device testing were unable to be completed. This will be further discussed in the next section of this report.

Based on the team's research and analysis, we believe that with further testing this device would be able to be competitive in the current market of septal closure devices.

Discussion

Due to the current COVID-19 situation, certain aspects of this project were unable to be completed. The two incomplete aspects include prototype manufacturing and device testing. Instead of completing the manufacturing and testing, we have developed a basic engineering package that includes directions for how these aspects would be completed in the future.

*Note that some of the engineering package repeats what is included in this report. The engineering package is included in this report for ease, but if distributed to a third party, would likely stand on its own. Table and figure numbers are separate from the previous tables and figures in this report.

Basic Engineering Package (BEP)

1. Device basic information and specifications

- a. The septal closure device is indicated for use in patients in need of a closure in the atrial septum, either from the effects of surgery or atrial septal defects.
- b. The device must be easy to implant, controlled by the physician, and have a long lifetime.
 - i. Specifications have been developed in order to meet these requirements

Table 1. Engineering Specifications

Factor	Specification 1	Specification 2
Easy Implantation	Adjustable sizing	Straight forward directions for use
Physician Controlled	Short implantation time	Compatible with current catheter/scope techniques
Long Lifetime	Materials that will not excessively degrade over time	Material will become ingrown in endothelium

- c. Specific engineering specifications were also developed in order to address the factors of stress failure, cost, and growth compatibility. These are shown in the table below.

Table 2. Engineering Specifications and Importance

Engineering Specs	Targets and Importance
Stress Failure	Must Withstand 40mmHg Pressure for simulated 100 years
Cost	Target: \leq \$250 per unit
Growth Compatibility	Target: \geq 75% encapsulation

- d. These specifications will be analyzed with more testing, which is discussed in the following sections

2. Prototype manufacturing

- a. The septal closure device prototype will consist of the following materials
 - i. Nitinol scaffolding
 - ii. PTFE patch
 - iii. Metal to metal epoxy (non-medical grade)
 1. The TCS anti-infection agent will not be included in the basic prototype
- b. This prototype will allow the team to better understand how the nitinol scaffolding will sit inside the PTFE patch
- c. The device will have 5 different sizes in order to cover all septal defects
 - i. 8 mm diameter
 - ii. 12 mm diameter
 - iii. 18 mm diameter
 - iv. 24 mm diameter
 - v. 28 mm diameter
- d. Each size is to be prototyped

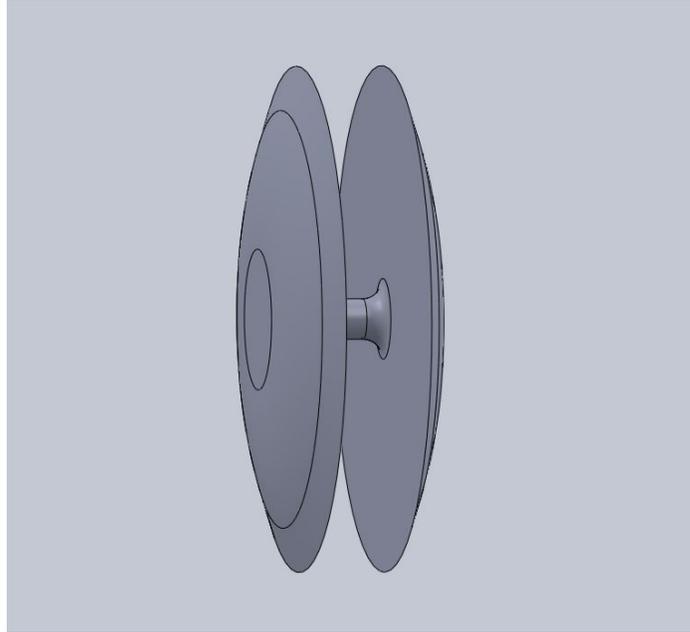


Figure 1. Solidworks design of septal closure device

3. Testing plans

- a. The device, based on our specifications, should have a lifetime of 50-100 years
- b. Simulations are to be run using COMSOL to test the lifetime and durability of the device
 - i. Simulations of 50 years, 75 years, 100 years
 - ii. To better understand how wear in a beating heart will affect device
- c. Plastic deformation not exceeding 1 mm after $2E9$ cycles will indicate the device is successful

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